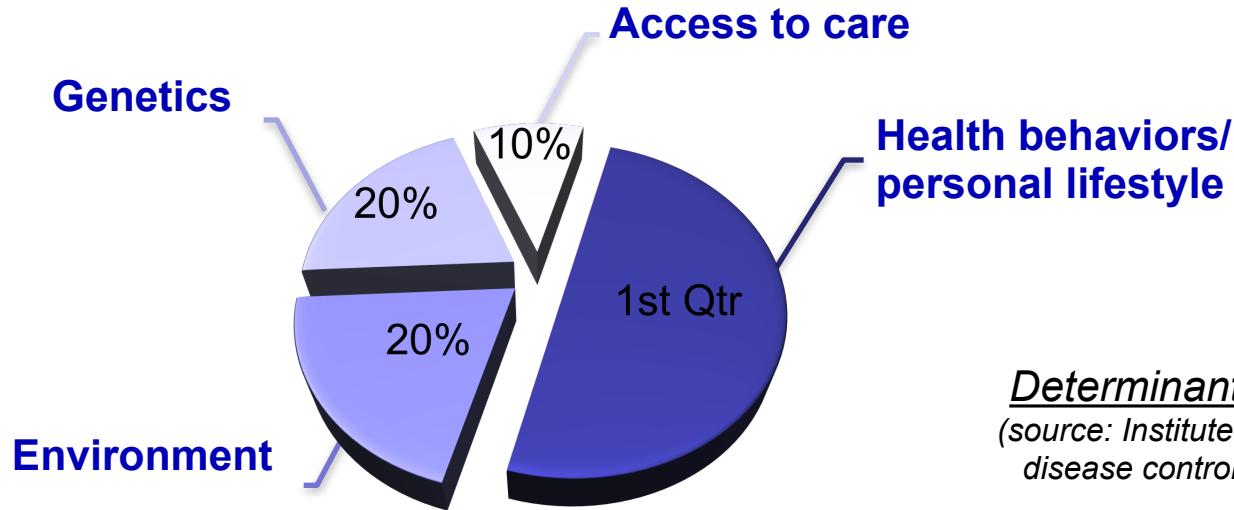


*Ultra-Low Power Design of
Multimodal Bio-Signal Wearable Systems*

Hossein Mamaghanian

***Embedded Systems Laboratory (ESL),
Laboratory of Signal Processing (LTS2)
EPFL, Switzerland***

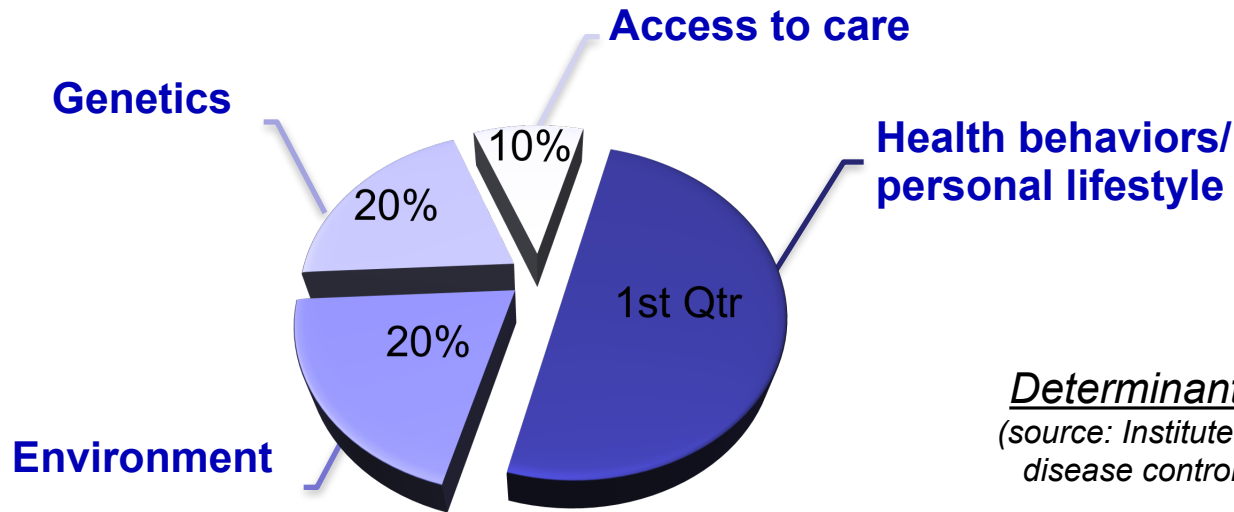
Pressing Changes in Healthcare Landscape and Economics Call for Personalized Healthcare



Determinants of health issues
(source: Institute for the future, Center for disease control and prevention, 2006)

- The burden of disease is shifting from diseases caused by infectious organisms to disorders with behavioral causes
- 50% of all deaths worldwide in 2006 and economic fallout in billions... expected to be 75% of gross domestic product by 2030

Pressing Changes in Healthcare Landscape and Economics Call for Personalized Healthcare



- The burden of disease is shifting from diseases caused by infectious organisms to disorders with behavioral causes
- 50% of all deaths worldwide in 2006 and economic fallout in billions... expected to be 75% of gross domestic product by 2030
- This calls for a two-fold paradigm shift in health delivery:

Symptom-based



Preventive healthcare

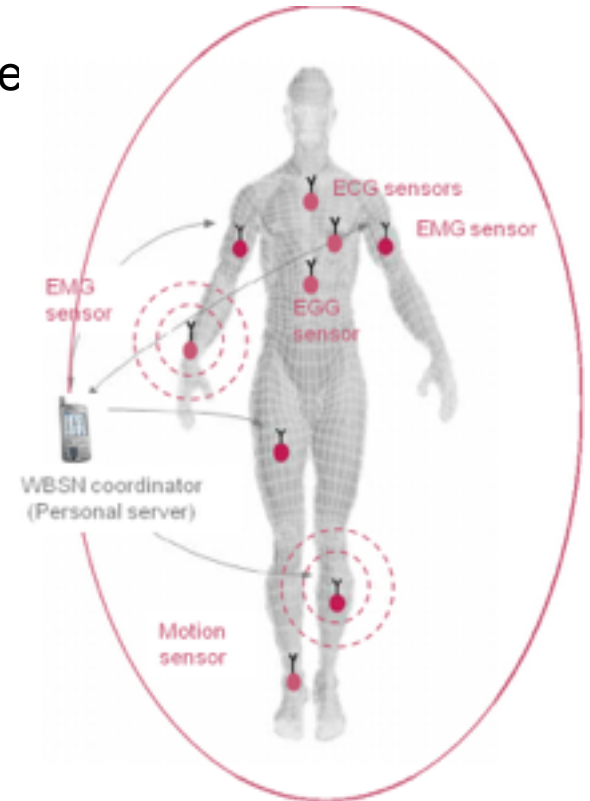
Hospital-centered sickcare



Person-centered healthcare

WBSN is a major technology for wearable personal health systems

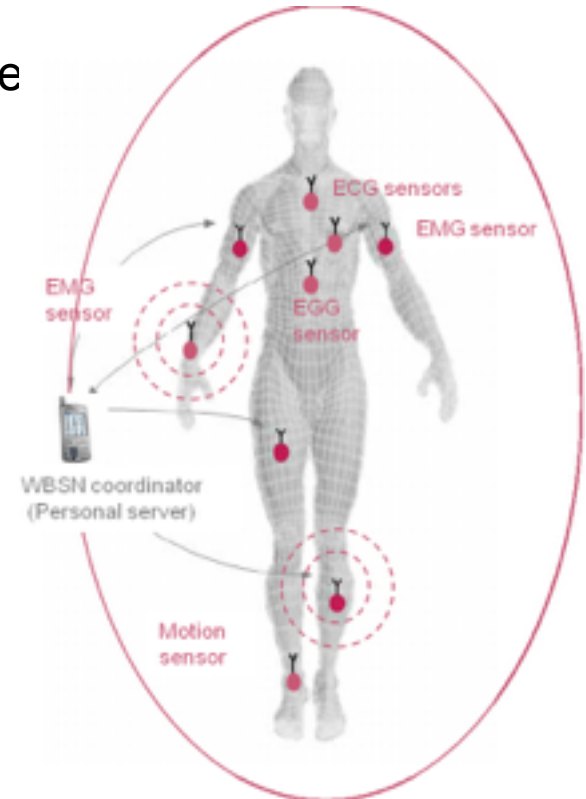
- Outfitting people with sensor collecting vital signals.
 - Many sensor: ECG, EMG, EEG, Acceleromete
 - Huge bandwidth required
 - High power consumption
 - Increasing demand for long time monitoring
 - Autonomy and lifetime



Wireless body area network
(WBSN or WBAN)

WBSN is a major technology for wearable personal health systems

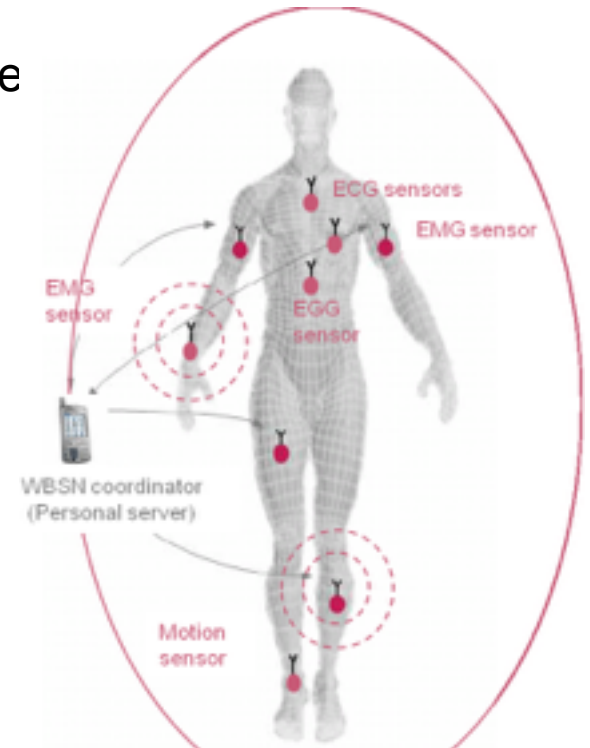
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 - bandwidth ✓
 - small in form factor, light in weight



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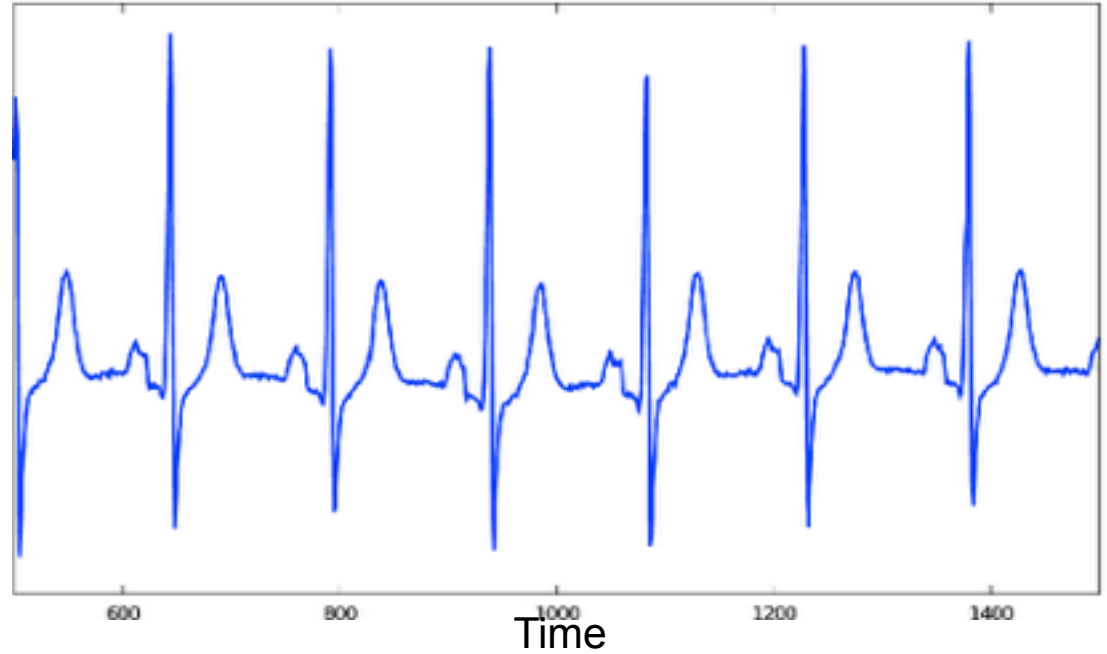
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Multi-parametric bio-signals
analysis:
How to design a WBSN?



Voltage



**Long-term ECG monitor
(Holter or event recorder)**

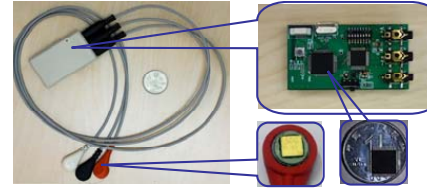
State-of-the-Art WBSN Designs: Streaming of Raw Data



Long-term ECG monitor
(Holter or event recorder)



MyHeart (Luprano,2006)



Kai,2011

Shimmer (2011)



Toumaz digital plaster (2011-13)

Streaming of only raw biosignal data



Health@Home (Sánchez, 2010)



MobiHealth (Halteren,2004)



TEMPO (Barth,2009)



Thiemjarus (2005-11)

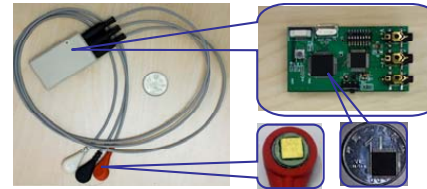
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Thiemjarus (2005-11)

Since the WBSN nodes do not do any processing,
how much can they last? Only 2-3 days...

- **TI MSP430 microcontroller**
 - 16-bit, 8MHz, 10KB RAM, 48KB Flash
 - ADC converters, DMA, HW multiplier
- **CC2420 radio**
 - 250 Kbps, ZigBee compliant
- **Sensors**
 - 3-channel ECG
 - Accelerometers and gyroscopes

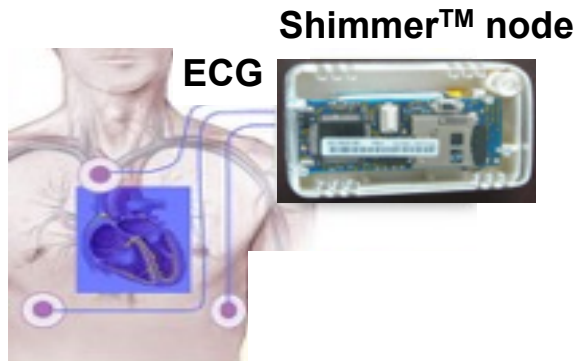


The Shimmer™ WBSN platform

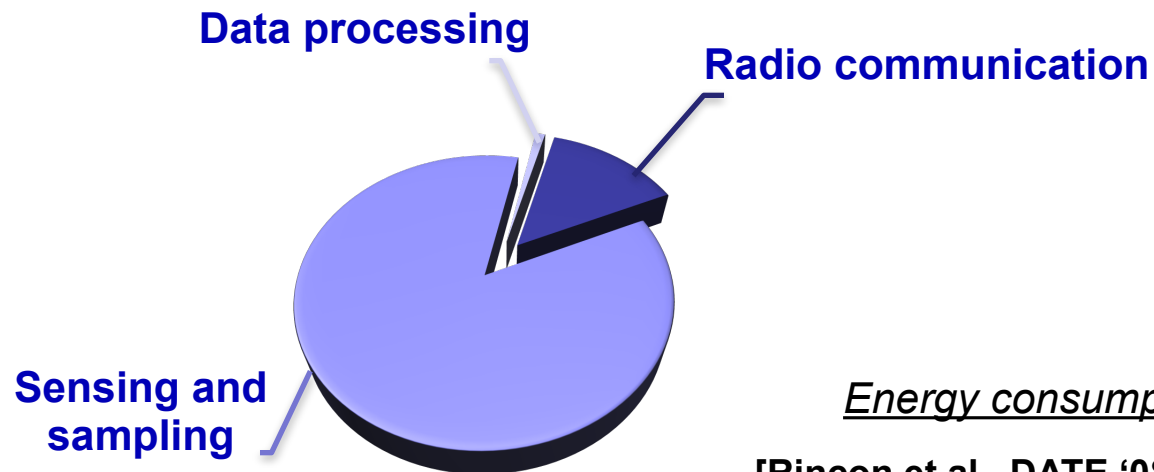
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 - 250 Kbps, ZigBee compliant
- **Sensors**
 - 3-channel ECG
 - Accelerometers and gyroscopes
- **CONSTRAINTS:**
 - No floating point operation
 - No hardware division
 - Limited memory
 - Limited autonomy (rechargeable Li-polymer battery of 380 mAh)



Long-lived wireless ECG monitoring require a major breakthrough in the energy efficiency of WBSN nodes



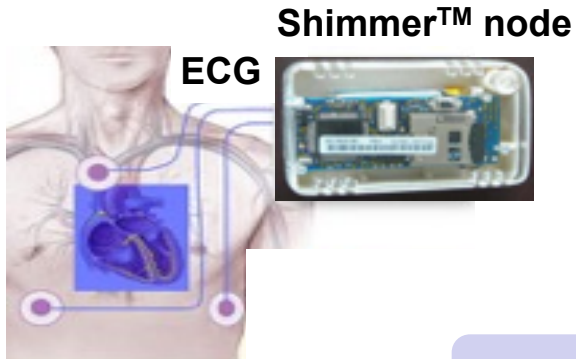
- This wireless 1-lead ECG streaming monitor **lasts 134.6 h.**



Energy consumption breakdown

[Rincon et al., DATE '08 and TITB '11]

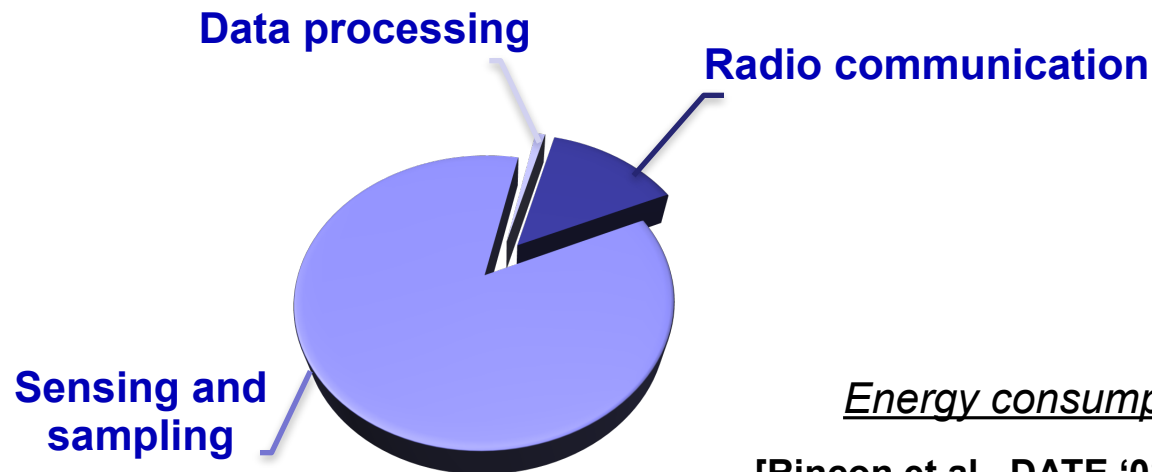
Long-lived wireless ECG monitoring require a major breakthrough in the energy efficiency of WBSN nodes



1. Can we reduce the data sensing/sampling cost and the amount of streamed data?
2. Can we embed automated analysis without compromising the system lifetime?

Under stringent processing and memory constraints!

- This wireless 1-lead ECG streaming monitor **lasts 134.6 h.**



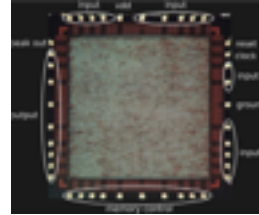
Energy consumption breakdown

[Rincon et al., DATE '08 and TITB '11]

State-of-the-Art **Smart** WBSN: Embedded Processing



Shimmer
(shimmerresearch, 2010-13)



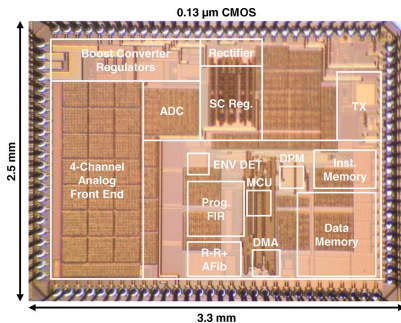
Heart Rate Monitoring
(Massagram, 2010)



Corventis's PiiX
(Corventis MCT systems, 2011-13)



Toumaz's Sensium Life
(Wong,2009)



Zhang (2012)



IMEC cardiac patch
(Yazicioglu,2009)



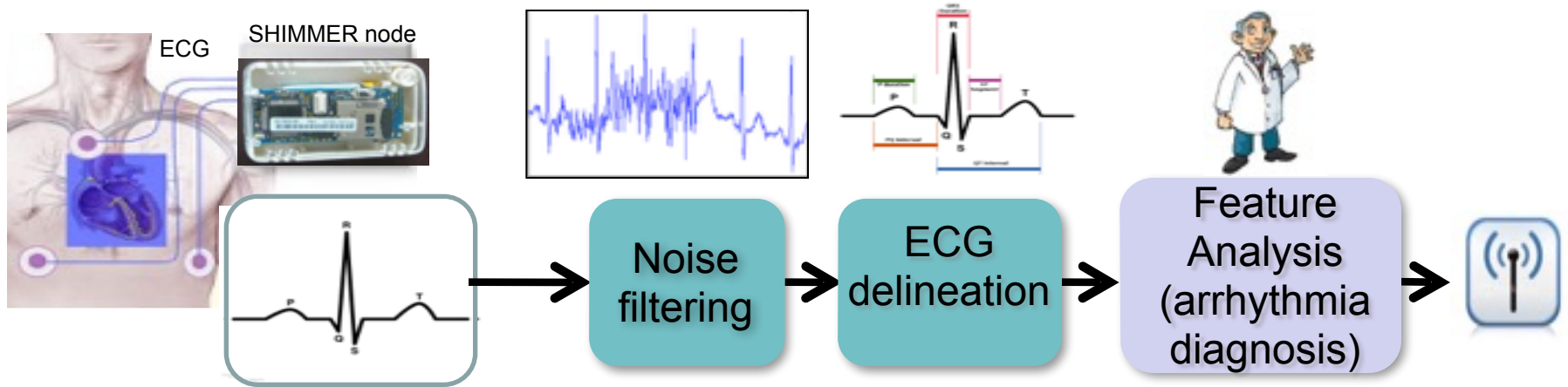
Holst Centre
(Masse, 2010-13)

Only simple filtering and one-lead input

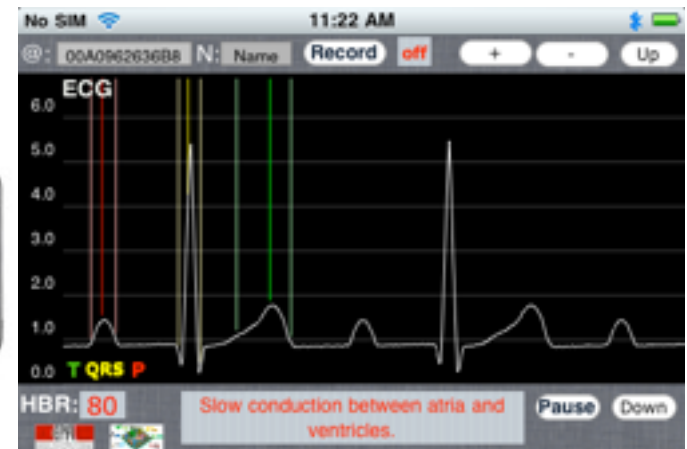
The goal from an ULP system-level perspective is to design:

- (1) Long-lived and accurate multi-lead ECG monitoring
- (2) Smart wireless personal health analysis systems

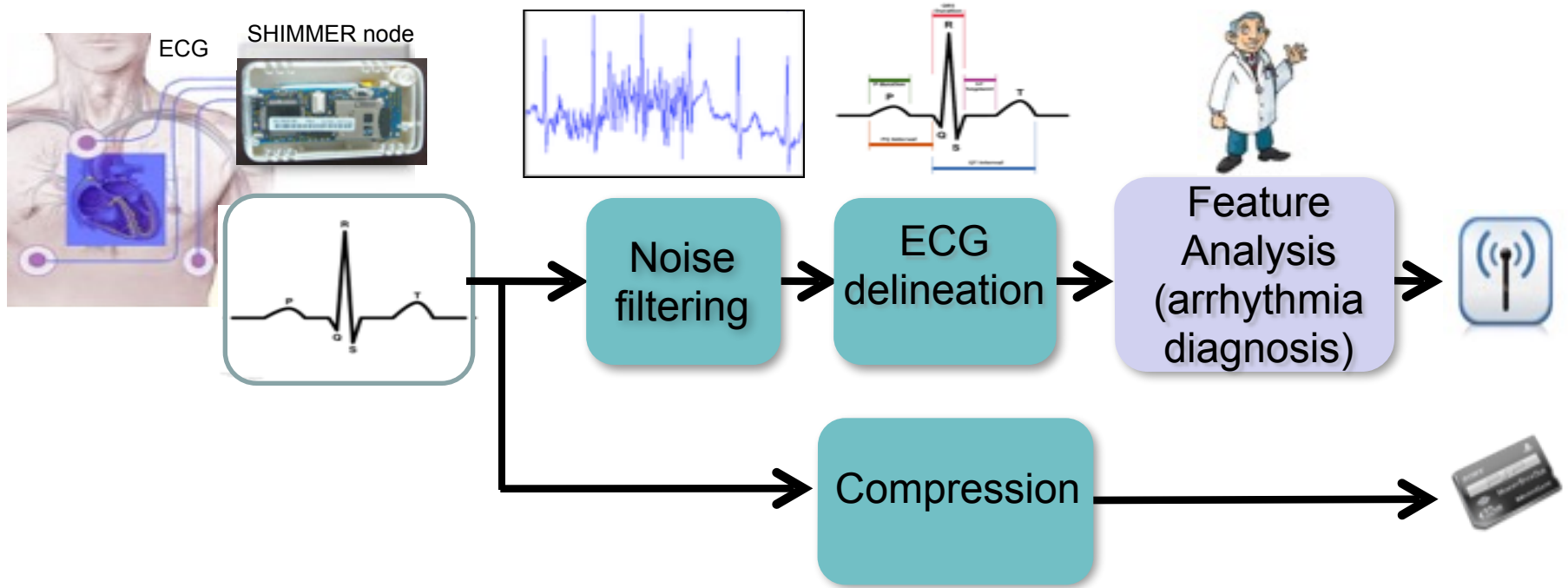
Our smart ECG sensor node concept for WBSN will capitalize on all 3 automatic processing algorithms



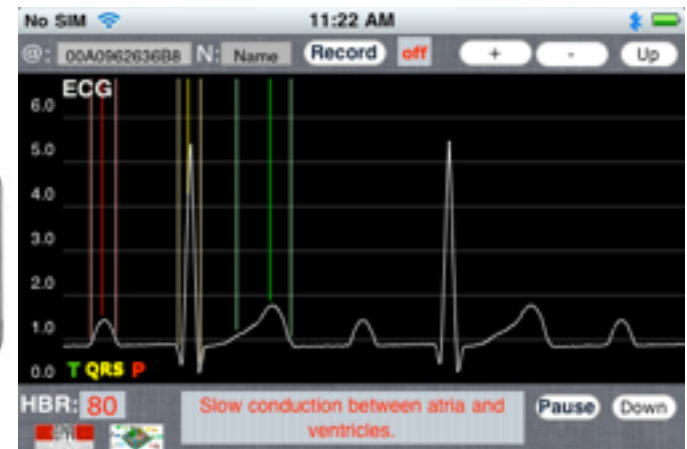
Displays the received data



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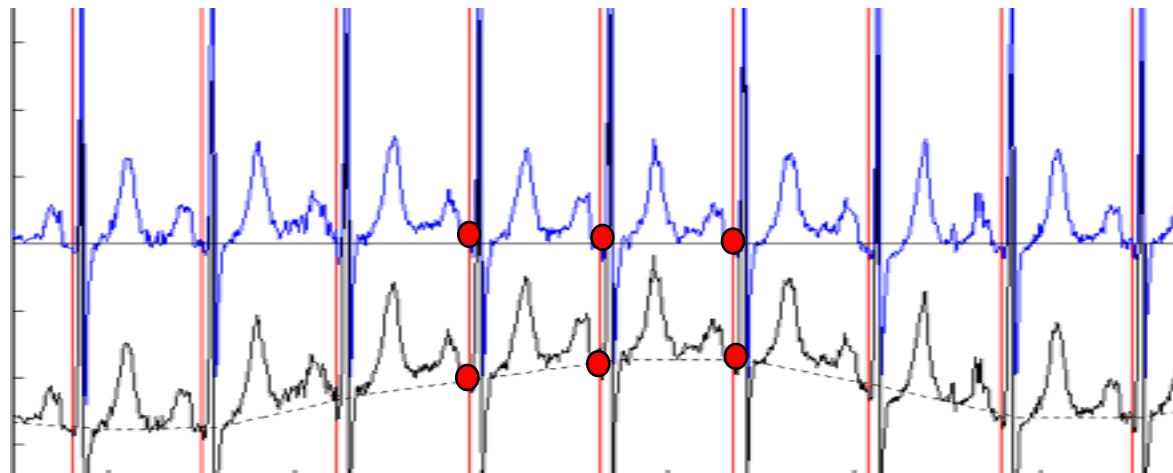
Selecting ECG filtering algorithms

■ Baseline wander and muscular noise removal

1. Cubic spline

[Rincon et al., TITB'11]

- Detect the knot of 3 consecutive beats
- The curve fitting the 3 knots is the baseline wander



Selecting ECG filtering algorithms

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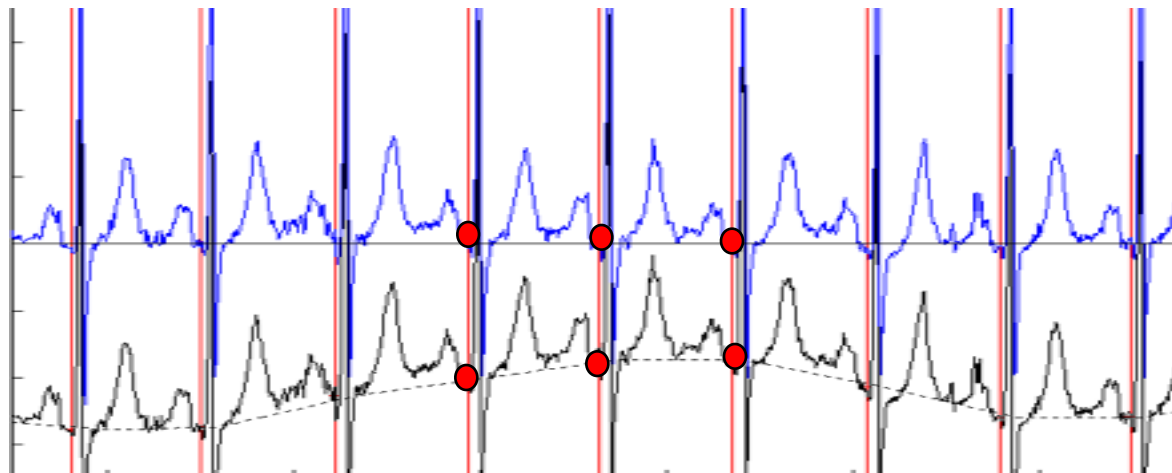
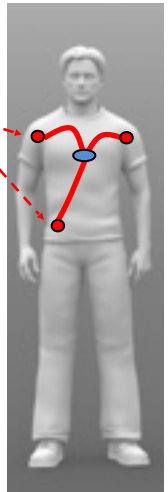
[Rincon et al., TITB'11]

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2. Morphological filtering (**99.2% accuracy**)

- Based on erosion and dilation operations
- Baseline correction + noise reduction

sensors



Selecting ECG filtering algorithms

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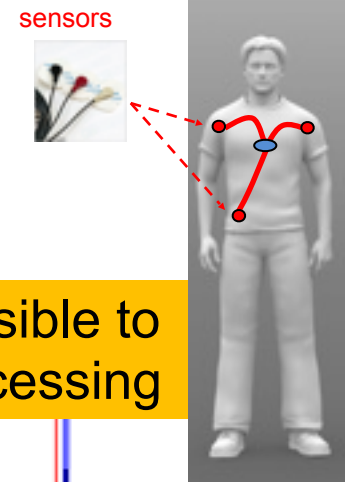
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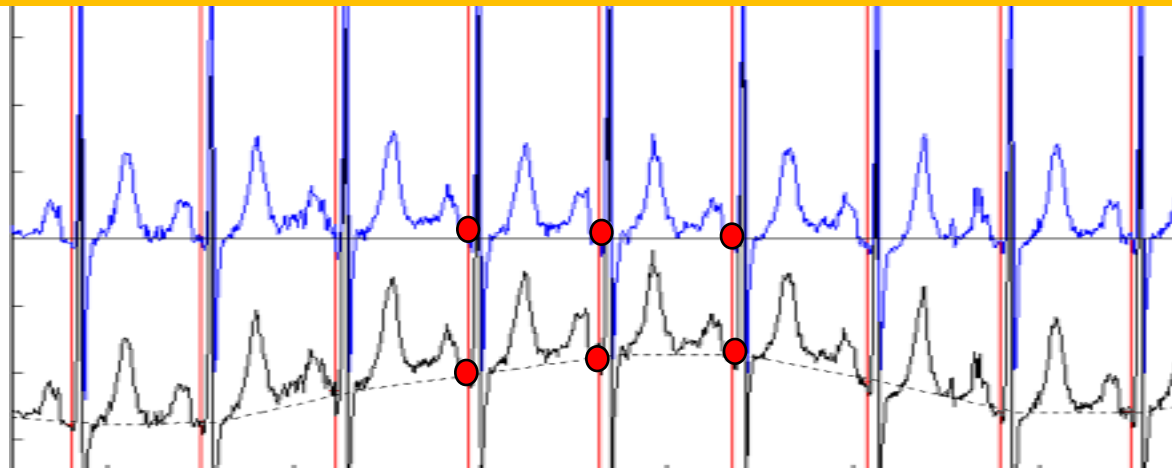
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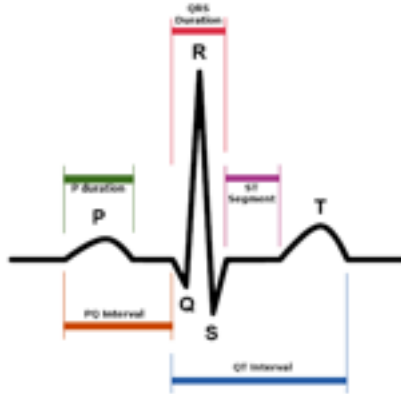
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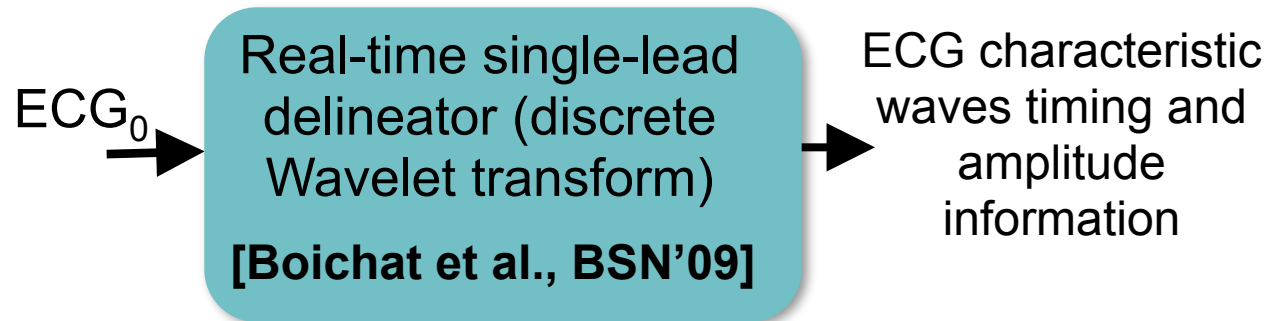
Moral of the story: knowing possible noise sources, possible to correct them with few sensors and “simple” signal processing



Embedded delineation of ECG characteristic waves

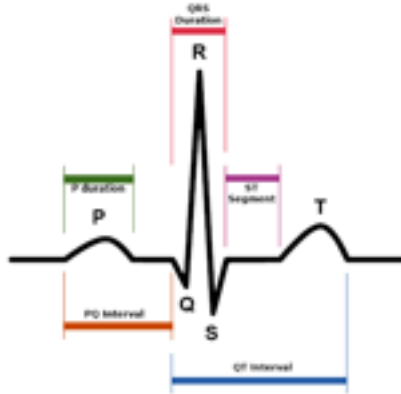


- Delineation is either done manually (by a cardiologist) or automatically (either by a bulky bedside equipment or offline on a PC)
- Delineation can be either based on a single lead or multiple leads

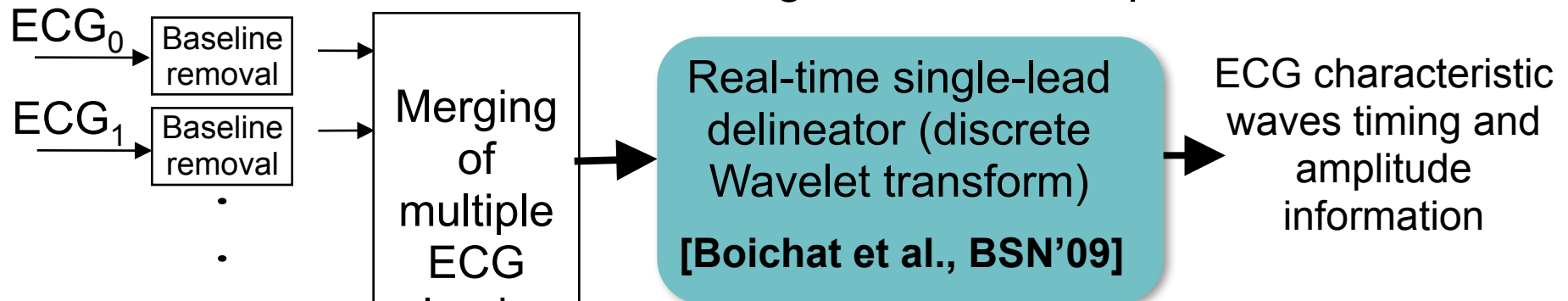


- **Optimizations for online operation:**
 - Processing of short blocks of ECG samples
 - Dynamically adapting underlying signal thresholds
 - Integer operations for fast implementation of complex functions ($\sqrt{\quad}$)

Embedded delineation of ECG characteristic waves



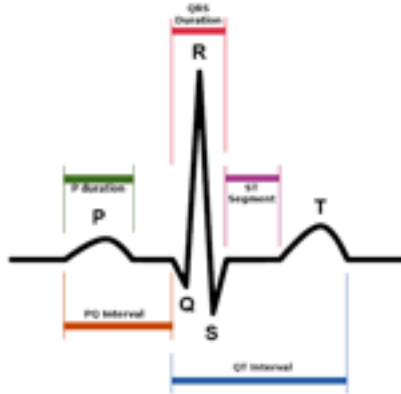
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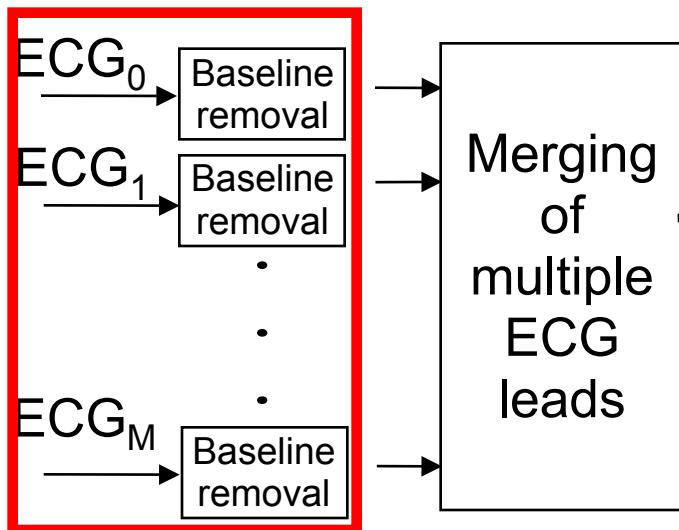
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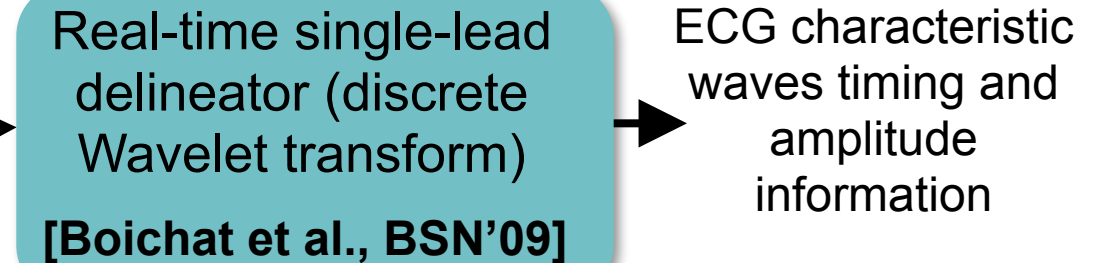


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Filtering

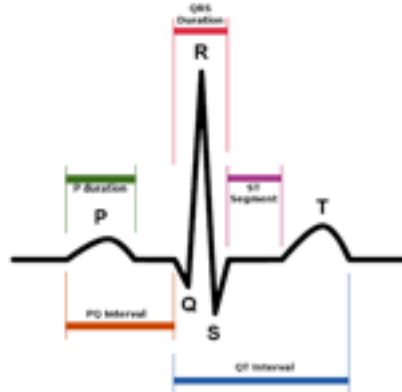


[Rincon et al., TITB'11]



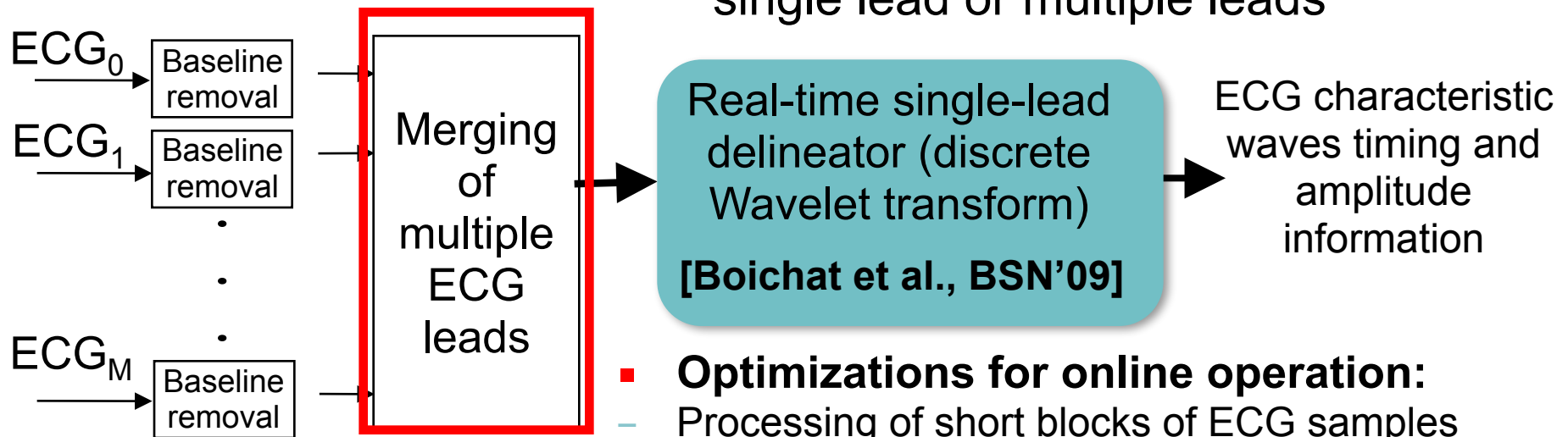
- **Optimizations for online operation:**
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Embedded delineation of ECG characteristic waves



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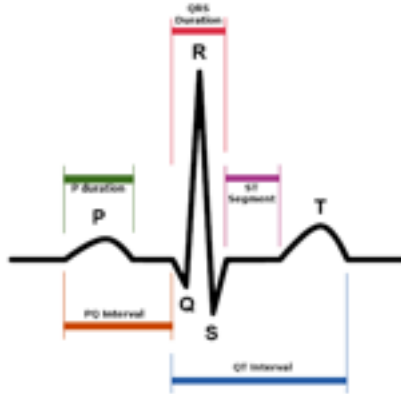
Root-mean-squared Delineation can be either based on a single lead or multiple leads



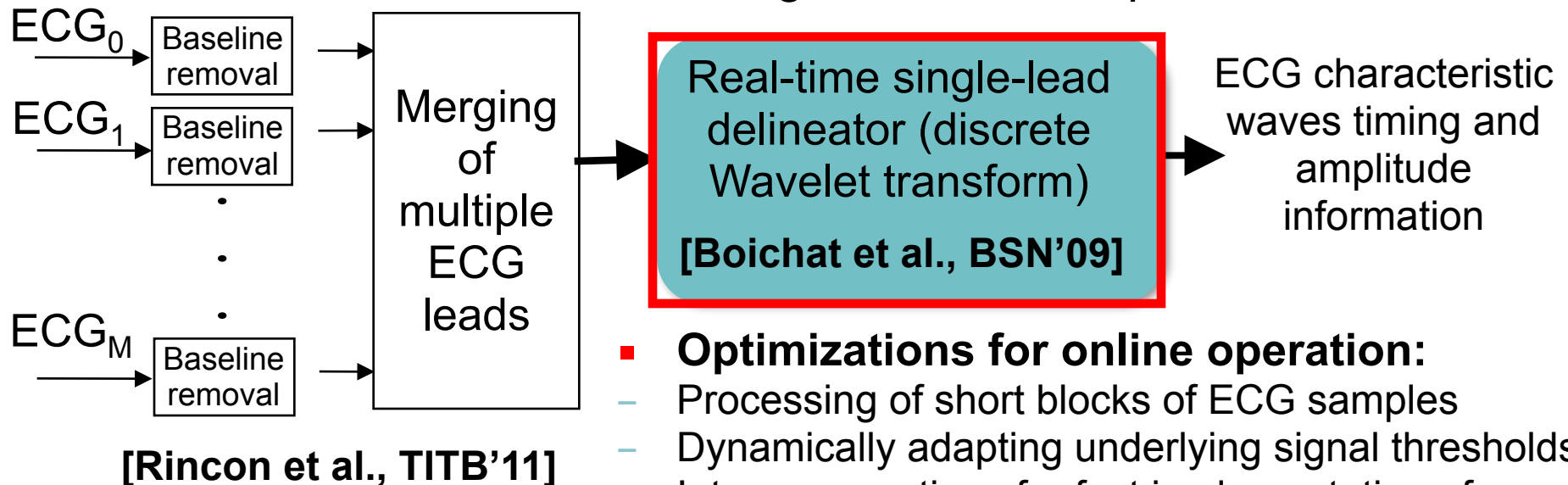
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Arrhythmia detection in WBSN systems

- Database of pathologies based on delineated points and thresholds
 - Defined at design time with doctors (few 100s of bytes of memory)
 - Applied at run-time by using a **simple look-up table**

$[QRS_{on}, QRS_{end}] \leq 0.10s$
 $0.12s \leq [P_{on}, QRS_{on}] \leq 0.20s$
 $T_{peak} > 0$
 $[QRS_{on}, R_{peak}] < 0.03s$
QT interval rule
HBR variability
Atrial activity



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 QT interval rule
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 Atrial activity



No issues of complexity or memory requirements, but need to develop **new adaptive classifiers** for each type of person

Biggest issue: Achieve efficient interaction with doctors!

See video at: <http://esl.epfl.ch/cms/lang/en/pid/46016>

A Real-Time Wavelet-Based Electrocardiogram Delineation System



- Real-time delineation demands limited requirements after careful algorithm optimization (computational load and memory footprint)

Algorithm	RAM usage	Buffers length	Execution time
Single-lead WT delineator	6.8 kBytes	512 elements	5%
Multi-lead WT delineator (morphological filter of baseline removal)	5.5 kBytes	256 elements	30.5% total (23% filtering, 2.5% multi-lead merging, 5% delineation)

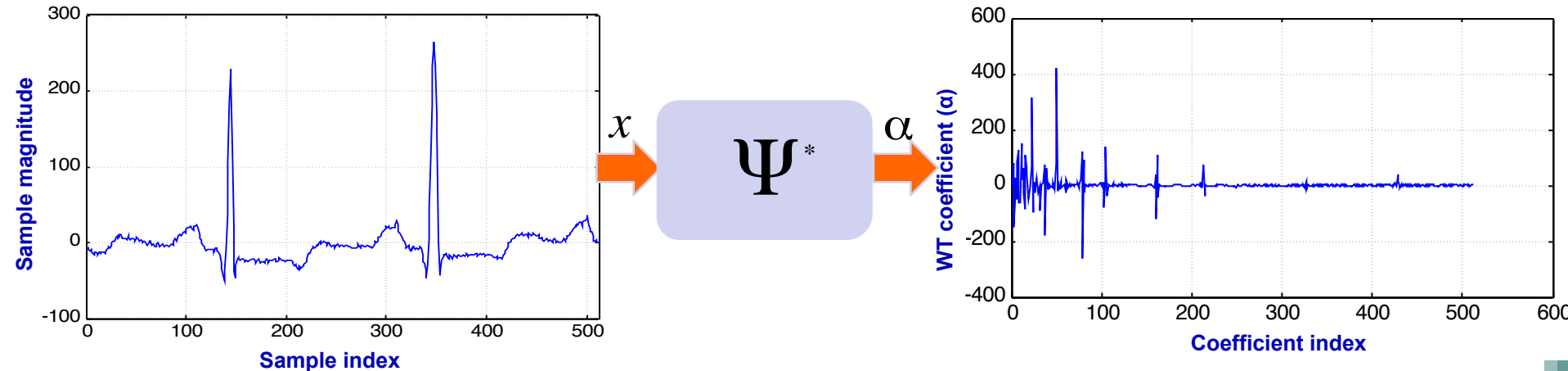
Execution of complex automatic ECG processing algorithms is possible

Small on-chip memory (10 kB) is the current limiting factor

Advanced on-chip processing gives real-time information about heart health with no impact on node lifetime: **more than 139 hours**

The electrocardiogram is a highly compressible signal

- ECG is highly sparse in the wavelet domain



- The Discrete Wavelet Transform (DWT) allows near-optimal compression of ECG signals

Orthogonal wavelet basis

Original ECG vector

$$x_N = \Psi \alpha_N$$

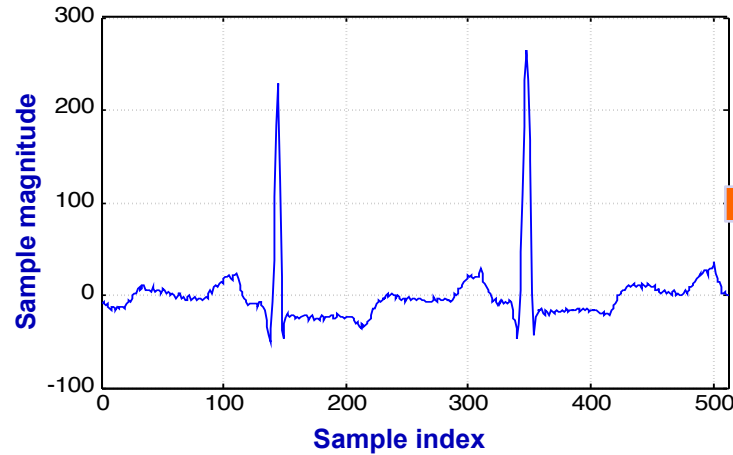
$$\|\alpha\|_0 = K \ll N$$

Coefficient vector

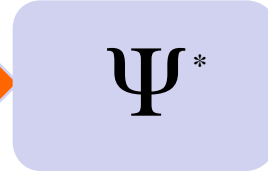
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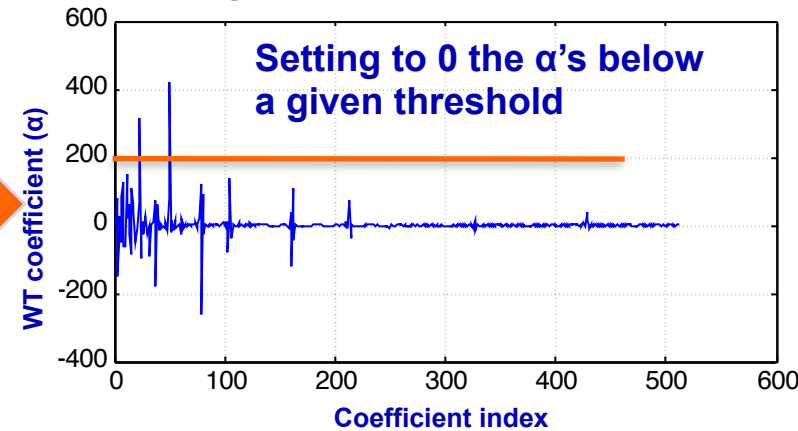
Thresholding-based DWT compression



x



α



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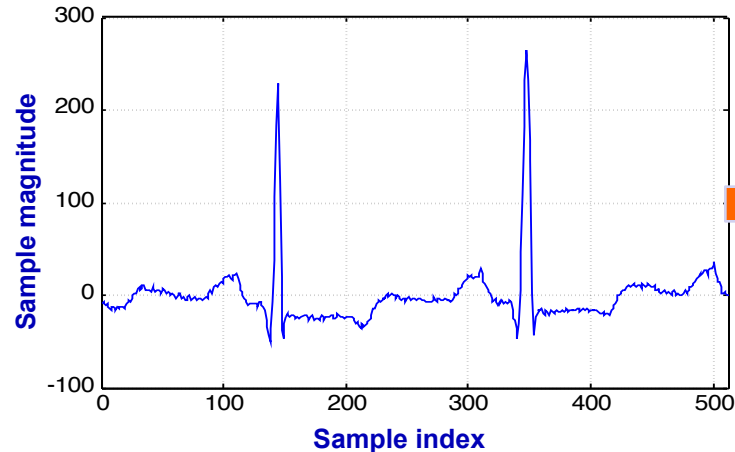
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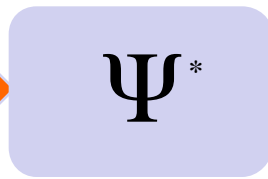
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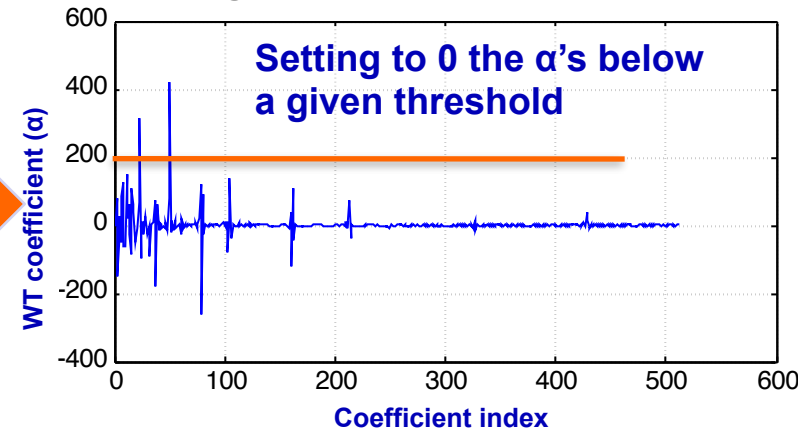
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$$x_N = \Psi \alpha_N$$

$$\|\alpha\|_0 = K \ll N$$

Coefficient vector

But can we create a “universally optimal” low-complexity compression scheme for ECG signals that works as well?

Compressed sensing (CS) is a new low-complexity sensing and compression paradigm for sparse signals

- Using CS it is sufficient to collect M ($\ll N$) linear random measurements (samples)
- Measurement/Sensing matrix
(Gaussian random matrix)**

$$y_{M \times 1} = \Phi_{M \times N} \cdot x_{N \times 1}$$

Measurement vector

Original ECG vector

- Then, α can be recovered by solving the convex optimization problem:

$$\min_{\alpha \in \mathbb{R}^N} \|\tilde{\alpha}\|_1 \quad \text{Subject to: } \|\Phi \Psi \tilde{\alpha} - y\|_2 \leq \sigma$$

Compressed sensing (CS) is a new low-complexity sensing and compression paradigm for sparse signals

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**Measurement/Sensing matrix
(Gaussian random matrix)**

$$y_{M \times 1} = \Phi_{M \times N} \cdot x_{N \times 1}$$

Measurement vector

Original ECG vector

CS is attractive for real-time ECG compression on resource-constrained WBSN, but what about biosignal degradation due to CS reconstruction (in real-time)?

- Then probl

$$\min_{\alpha \in \mathbb{R}^N} \|\tilde{\alpha}\|_1 \quad \text{Subject to: } \|\Phi \Psi \tilde{\alpha} - y\|_2 \leq \sigma$$

See video at: <http://esl.epfl.ch/page-42817.html>

A Real-Time Compressed Sensing (CS)-Based Personal Electrocardiogram Monitoring System

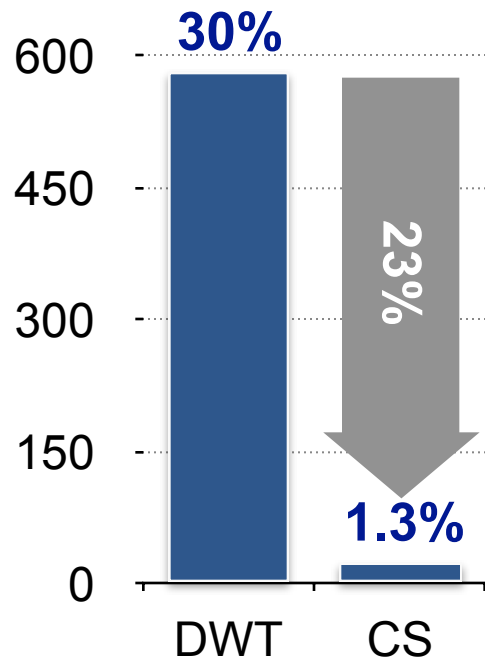


ÉCOLE POLYTECHNIQUE
FÉDÉRALE DE LAUSANNE



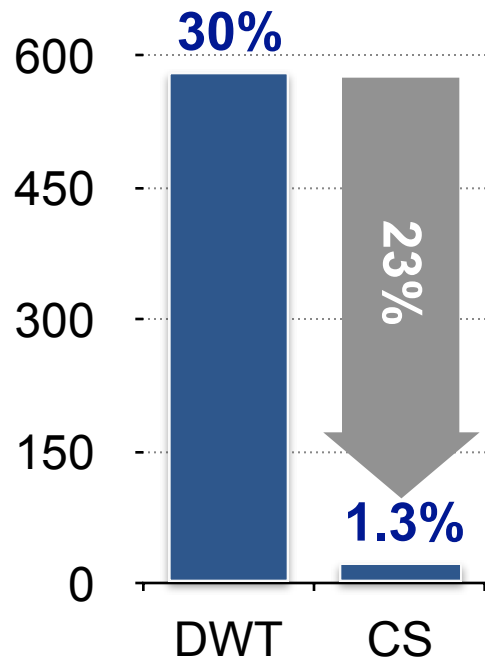
CS provides over a 23-fold reduction in execution time,
but only 10% node lifetime extension

Code execution time

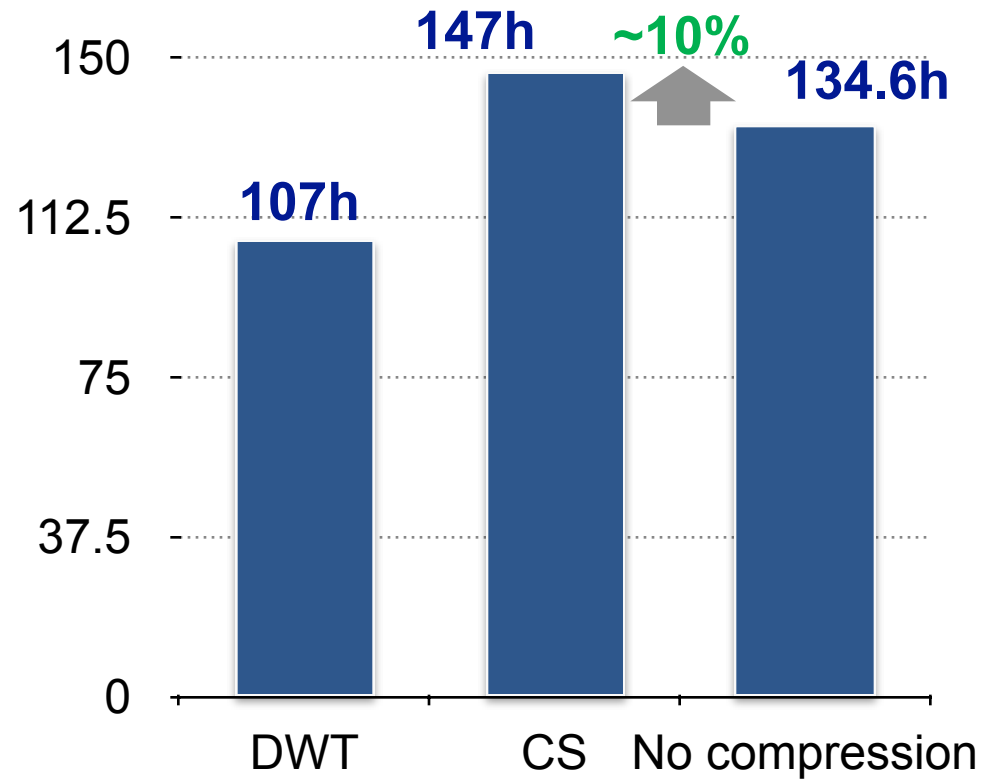


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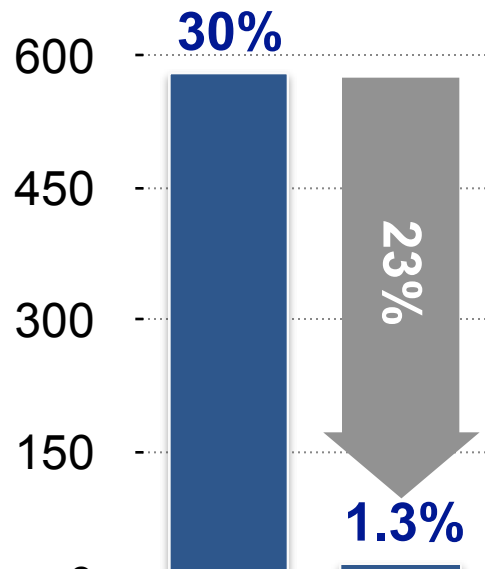


Node lifetime

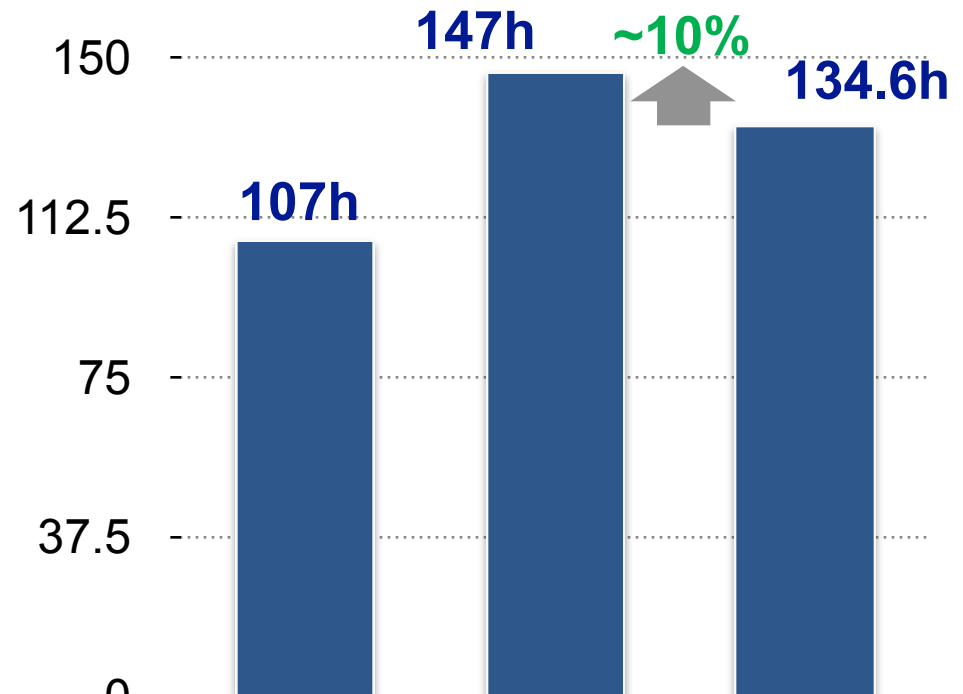


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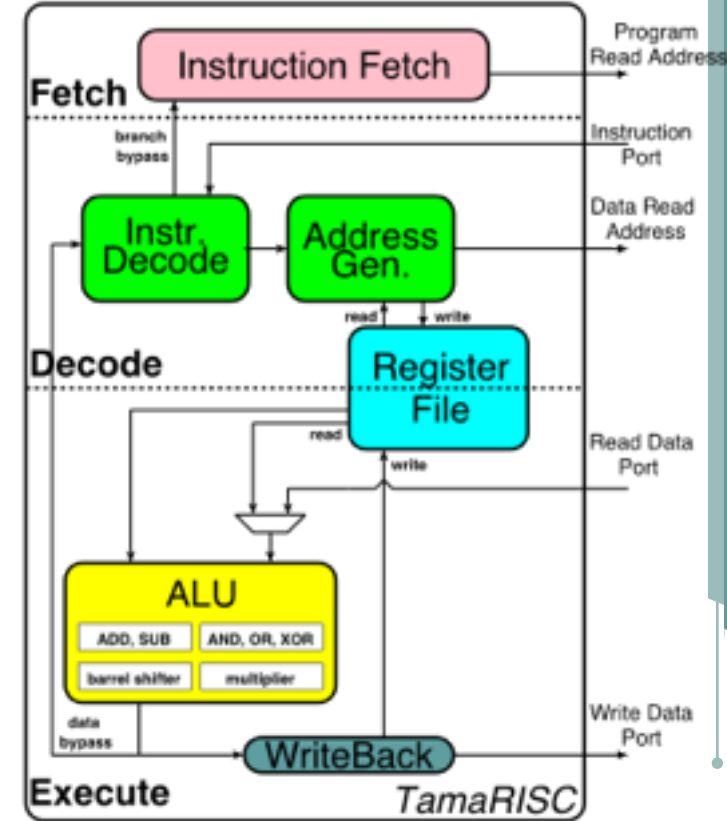
Node lifetime



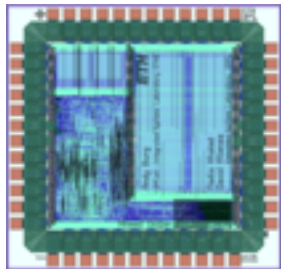
Limited gains because the used generic microcontroller is not optimized for ultra-low power **DSP and CS-based operations in biological signals**

Simplicity is the key: A new generation of ultra-low-power processing cores for WBSNs

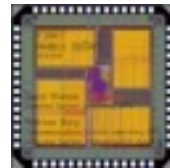
- FIRAT/TamaRISC: Inspired on PIC24
 - 16-bit RISC, simple 3-stage pipeline
 - Drastically reduced to 25 types of instructions (added CS execution support)
 - 1 cycle/inst., Immediate branch, full data bypass
 - Minimal ALU: ADD, SUB, AND, OR, XOR, Shift, Mult.
- Minimal area/power for biosignals processing
 - Less than 5% of an embedded platform (< 10 kGE)
 - Low-power computing: ~10 MHz (180MHz@1V)



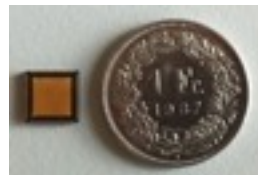
[Dogan et al., DATE 2012]



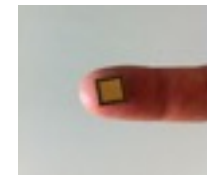
Dicle (umcL 180nm)



Firat (umcL 90nm)



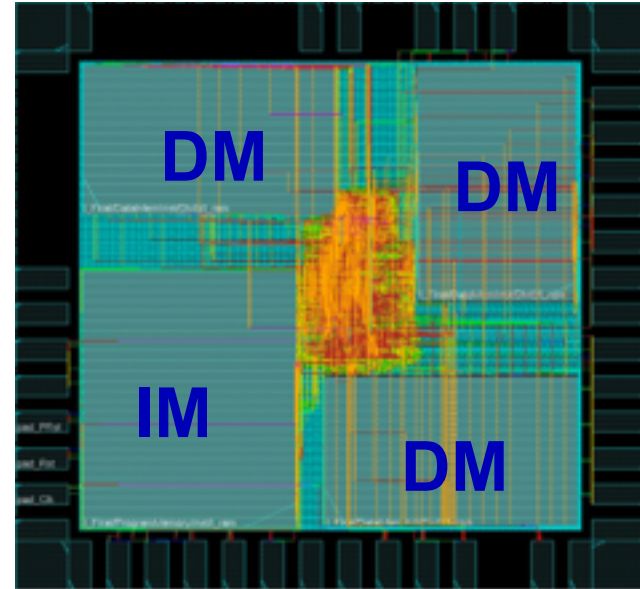
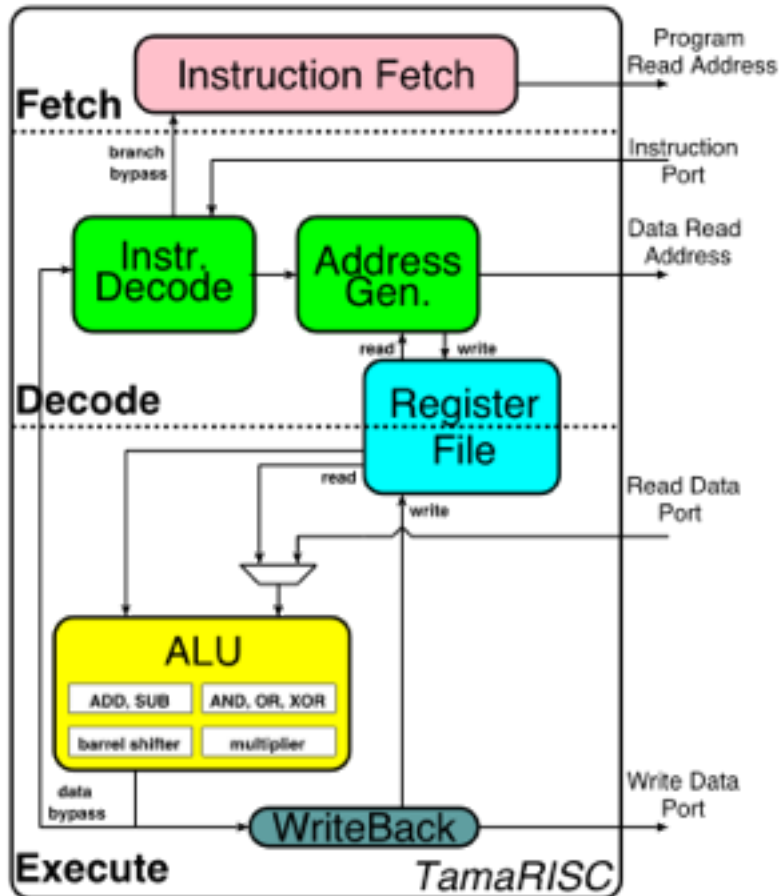
Firat ASIC vs. 1CHF coin



... And on a finger tip!

Simplicity is the key: TamaRISC processing core and memories

- Specialized 16-bit RISC for biosignals
 - But **memories are key**: 50% energy



- Low-voltage multi-banked memories
 - 32-kB instruction memory (IM)
 - 36-kByte data memory (DM)

[Dogan et al., DATE 2013]

[Dogan et al., DATE 2012]

TamaRISC: Experimental results

	Number of Clock Cycles(*)		
	FIRAT	TamaRISC	MSP430
Filtering-DWT	1.85M K	1.81M	4.7M
Compression	114K	90K	800K

(*) 1-package compression (512 samples)

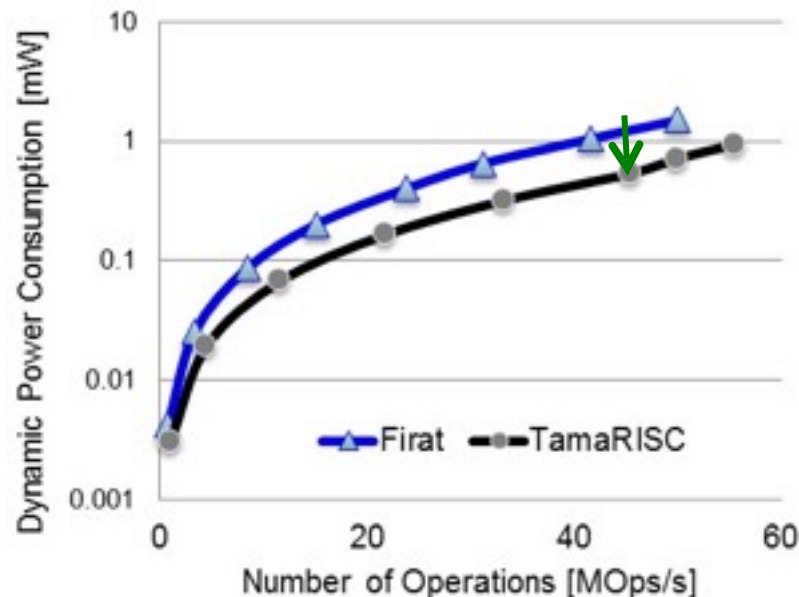
TamaRISC only 38% of MSP430 cycles due to architecture specialization and low voltage operation

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TamaRISC vs Firat: Faster and 30% extra power savings due to full data bypass, CS support and low-power encoding

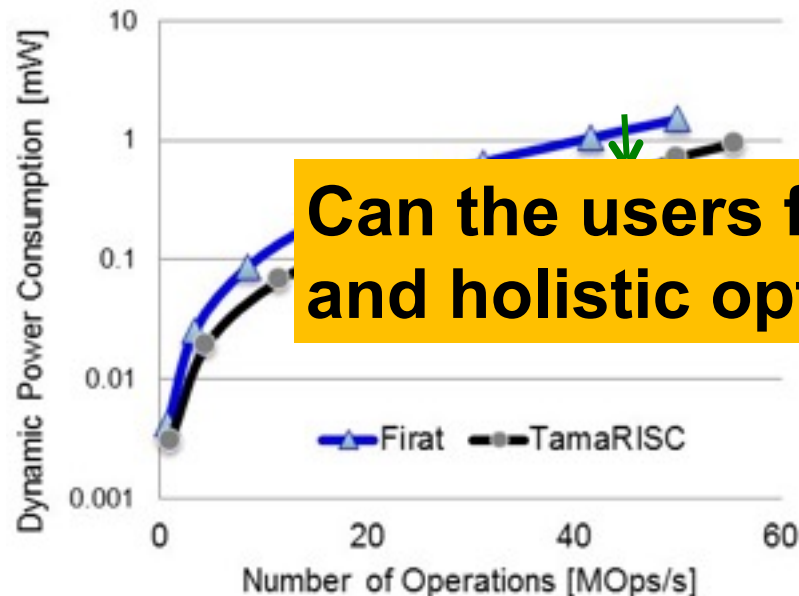
	Energy per Ops @ 1.0 V	Technology
TamaRISC	12.1 pJ	90 nm
16-bit [Kwong,2011]	> 47 pJ	130 nm
32-bit [Ickes,2011]	19.7 pJ-27 pJ	65 nm

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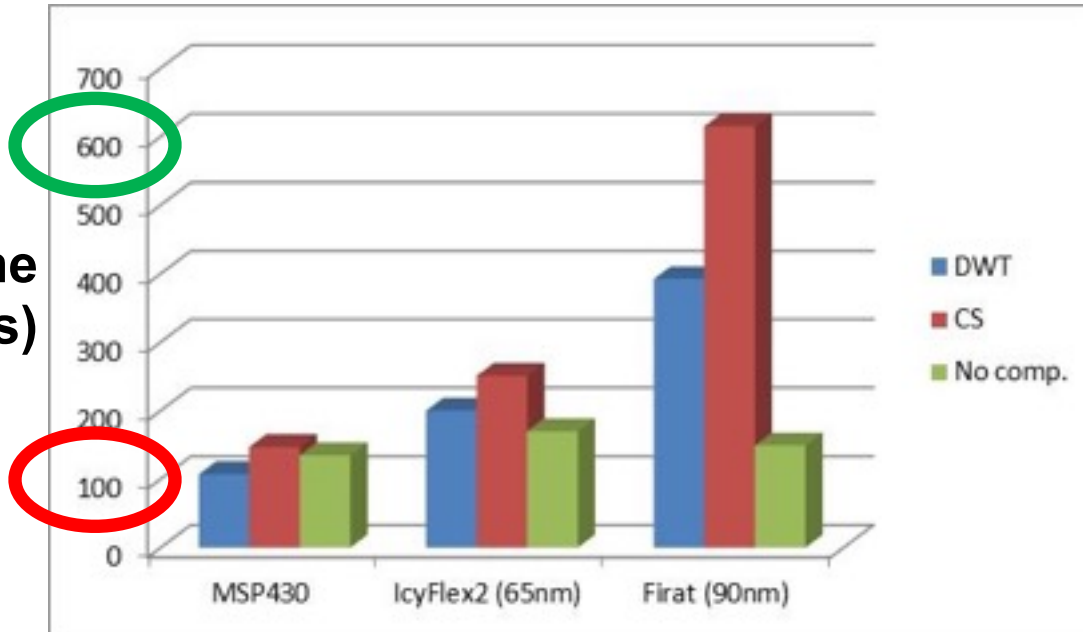
TamaRISC vs Firat: Faster and 30% extra power savings due to full data bypass, CS support and low-power encoding

Can the users finally see the benefit of CS and holistic optimization at system-level?

TamaRISC	12.1 pJ	90 nm
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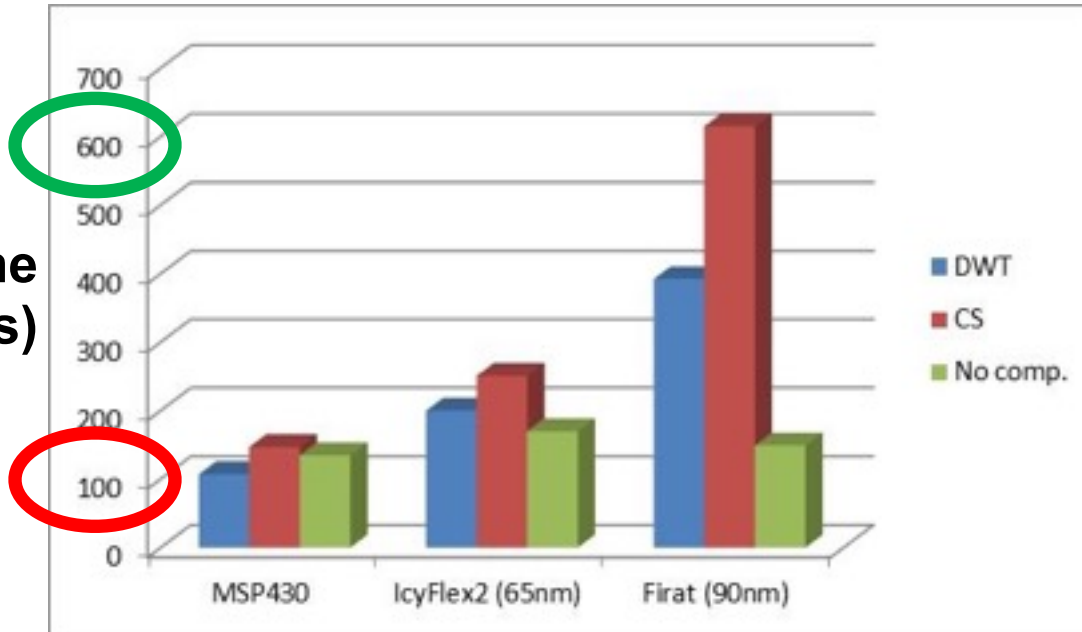
CS and biosignals algorithms analysis show true advantages on ultra-low-power (ULP) processors

**Lifetime
(in hours)**



CS and biosignals algorithms analysis show true advantages on ultra-low-power (ULP) processors

Lifetime
(in hours)



- Feasible to develop long-lasting smart WBSN nodes that interact with smartphones
 - Adapts at run-time to patient's heart
 - Automatic detection of arrhythmias
 - Real-time notification to doctors

SmartCardia



CS and biosignals algorithms analysis show true advantages on ultra-low-power (ULP) processors



See video at: <http://www.smartcardia.com>

Smart ULP WBSN designs can reach resonance in the media, but also impact in medical community!

18 octobre 2011
Le résumé de l'actualité romande



Date: 19.10.2011
LE TEMPS

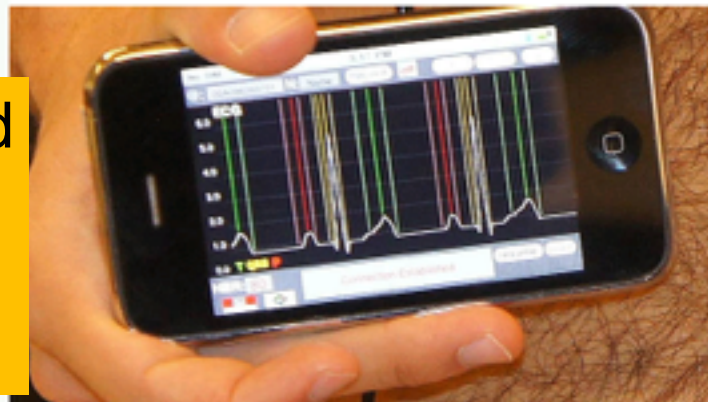
Santé

Notre cœur sur écoute



Smartphone detects danger in a heartbeat

By Matthew Knight, CNN
October 24, 2011 — Updated 10:14 GMT (05:14 PRC) | Filed under: [Mobile](#)



Date: 19.10.2011

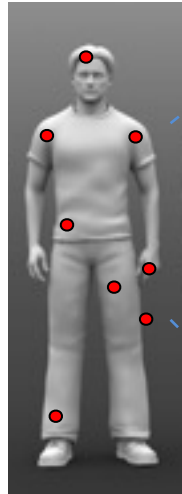
Blick

Ein SMS vom Herz

Lausanne – Diagnose: Herzinfarkt. Der häufigsten Todesursache der Welt wird der Kampf angesagt, und zwar mit Schweizer Technik. Forscher der ETH Lausanne haben ein Gerät entwickelt, das den Herzrhythmus konstant überwachen kann. Falls eine Rhythmusstörung auftritt, **sendet das Gerät an Patient und Arzt per SMS oder E-Mail eine Warnung.** «Das System liefert sehr präzise Daten und verfügt über einen leistungsfähigen Akku mit einer Laufzeit von drei bis vier Wochen», sagt Forscher David Atienza.

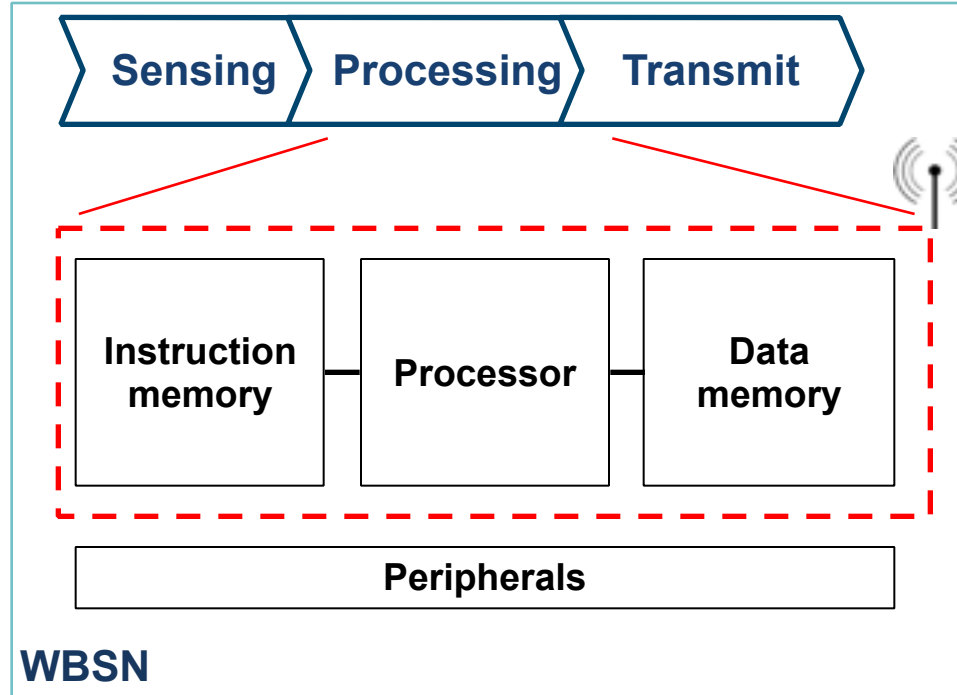
Non-intrusive, light and can reduce visits by 50-60% for patients (4-week test)

Next-Generation: “Really Smart” (or just Smarter) WBSN for Healthcare



Bio-signals

- ECG
- Blood pres.
- EEG
- Respiration
- Movements



Output:
Diagnose,
Abnormality,
Analysis
...

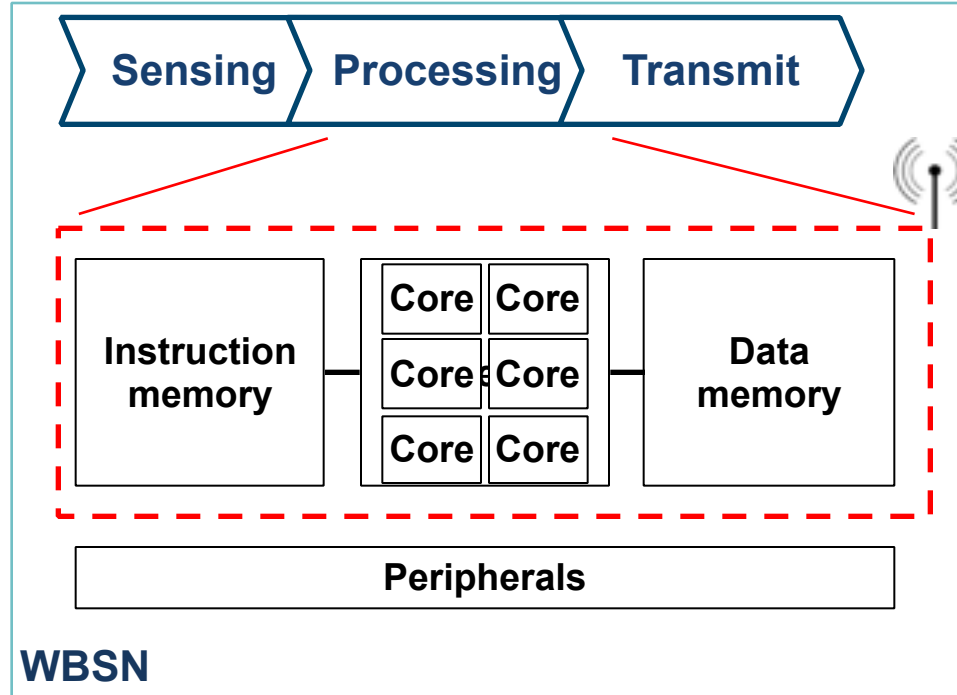
CAN WE DO BETTER?

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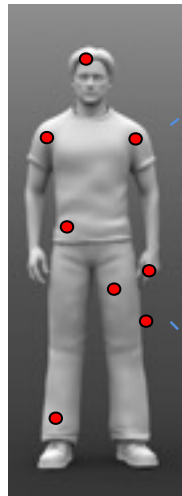
Output:
Diagnose,
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CAN WE DO BETTER?

HW

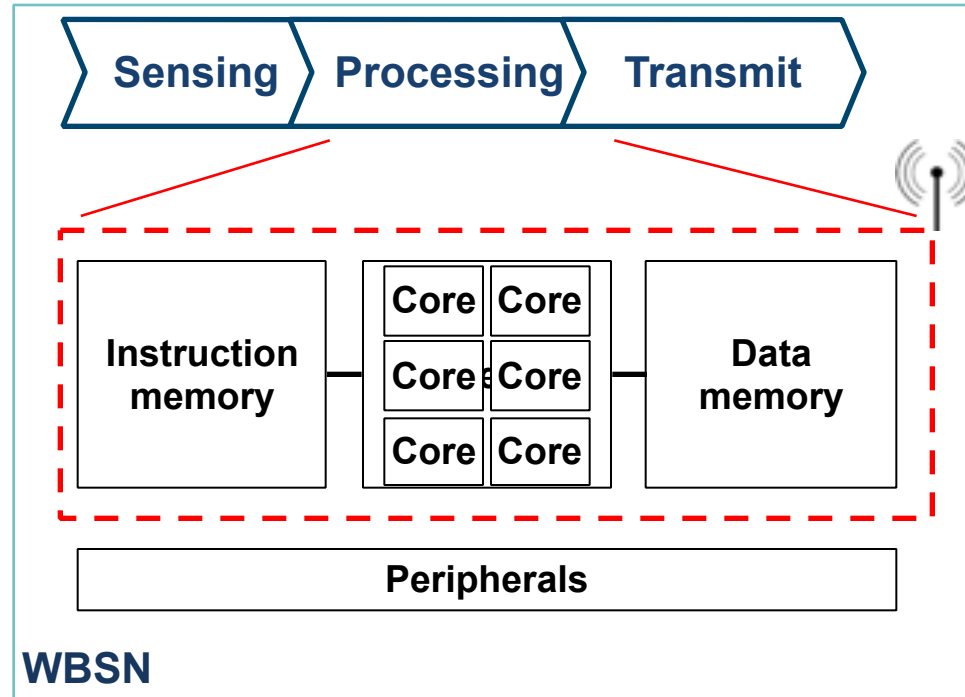
- Ultra-low Power (ULP) architectures
- Hybrid CS-based front end design

Next-Generation: “Really Smart” (or just Smarter) WBSN for Healthcare



Bio-signals

- ECG →
- Blood pres. →
- EEG →
- Respiration →
- Movements →



Output:
Diagnose,
Abnormality,
Analysis
...

CAN WE DO BETTER?

- Selective DSP (Classification)
- Multi-lead Compression

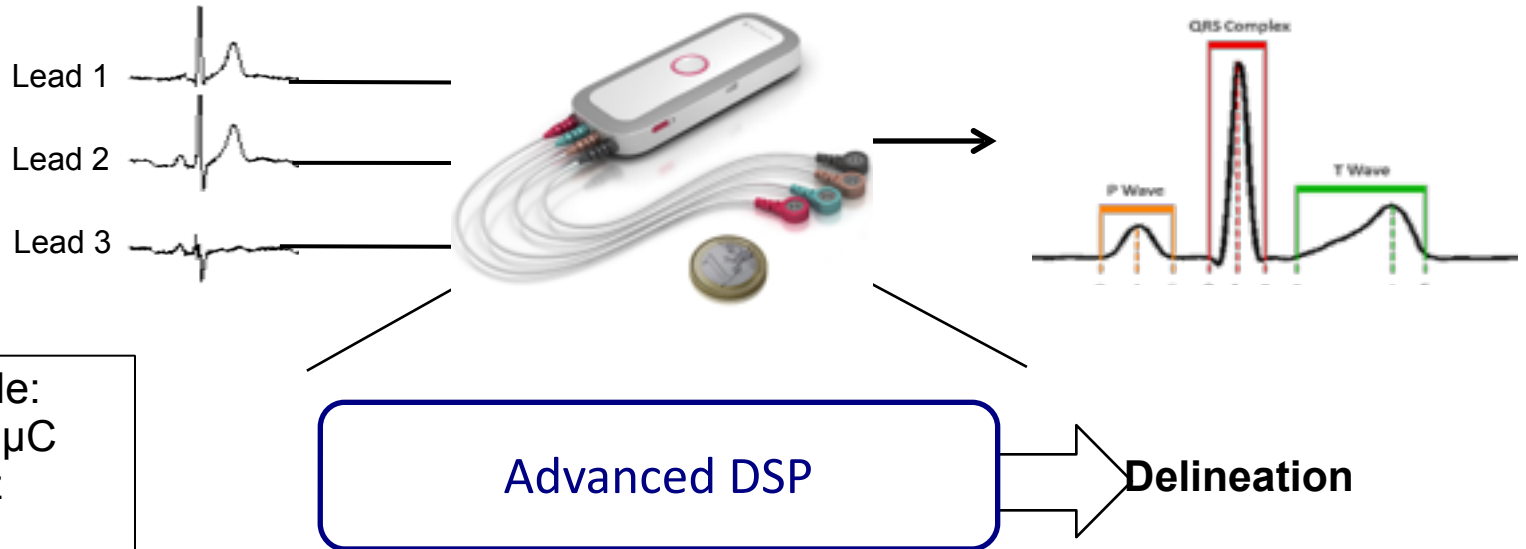
SW

HW

- Ultra-low Power (ULP) architectures
- Hybrid CS-based front end design

Let's exploit BIG DATA!

Selective advanced ECG analysis



WBSN Example:

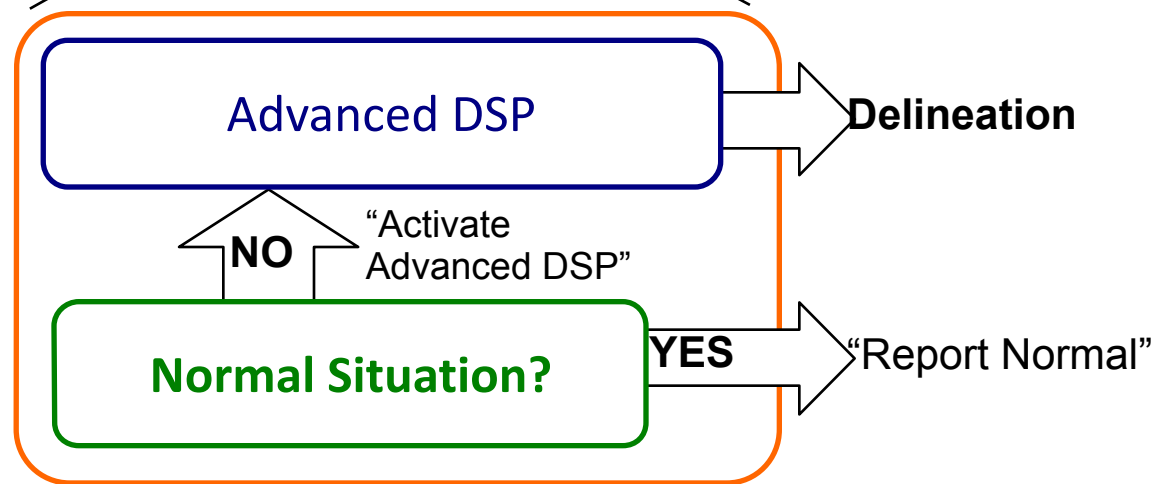
- TamaRISC μ C
 - 8 MHz
 - 16-bit
 - 128 KB
 - Flash
- CC240 radio
 - Zigbee
 - Bluetooth
- 480 mAh Battery
→ 1200h running

Selective advanced ECG analysis



WBSN Example:

- TamaRISC μ C
 - 8 MHz
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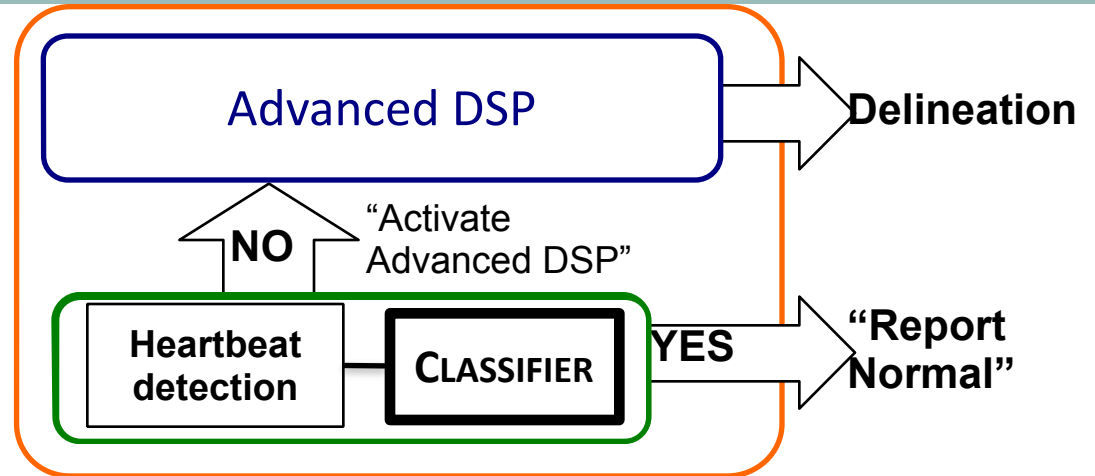
Possible Selective Activation?

Classification of Heartbeats

- Normal condition
 - Normal heartbeat morphology

Classif. heartbeats

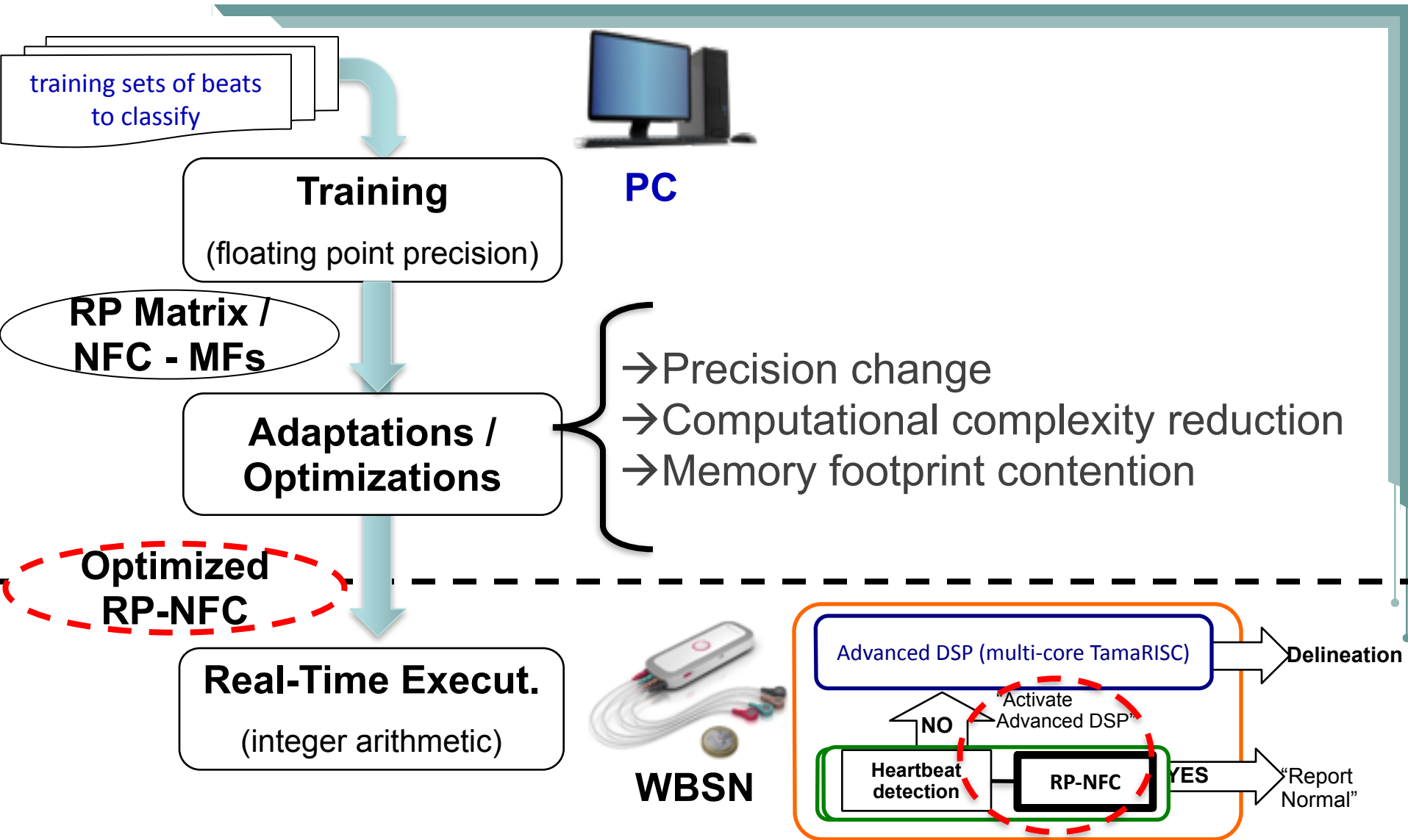
- Problem dimensionality
- Very complex existing algorithms



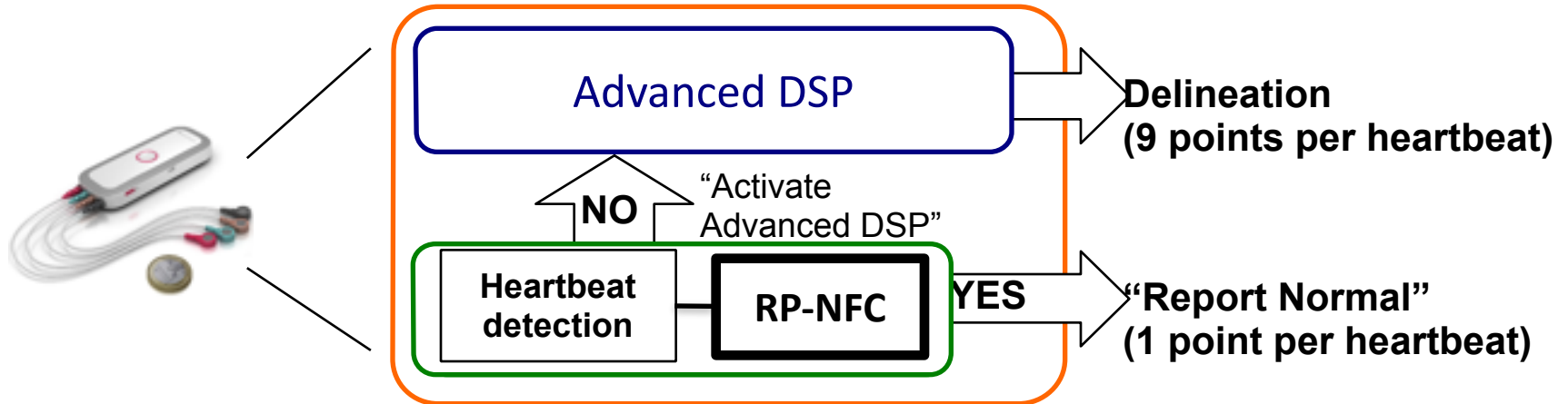
Light-weight embedded heartbeat classifier

1. Random Projection (RP) dimensionality reduction
2. Embedded Neuro-Fuzzy classifier (NFC)

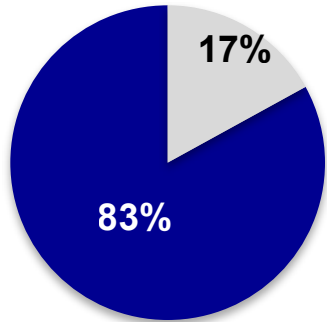
Proposed framework for next-generation WBSN designs



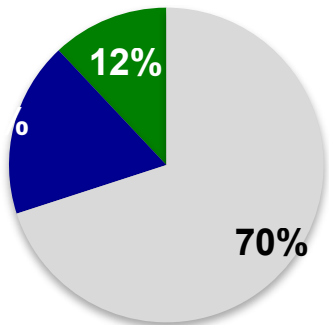
Initial Case study: Smarter ECG Monitor



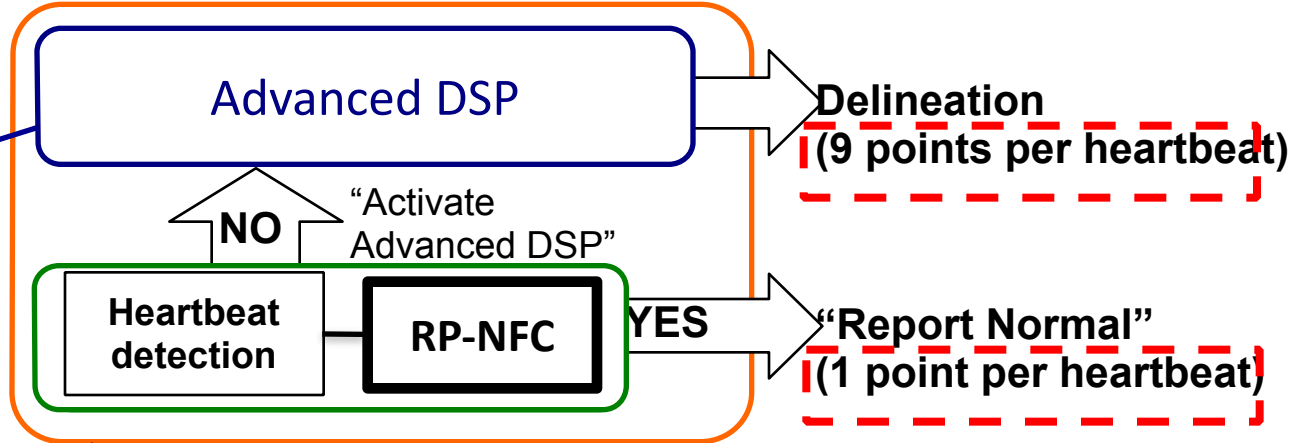
Initial Case study: Smarter ECG Monitor



Typical ECG Monitor

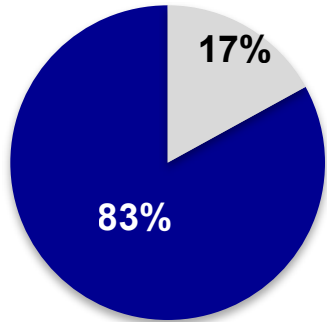


Smarter ECG Monitor



- Duty cycle reduction of 65% for MIT-BIH DB
- Transmission or storage reduction of 68%

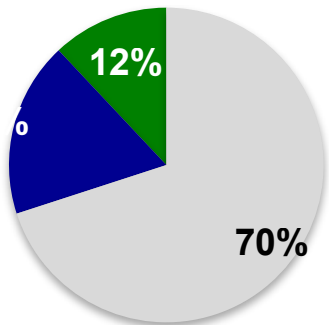
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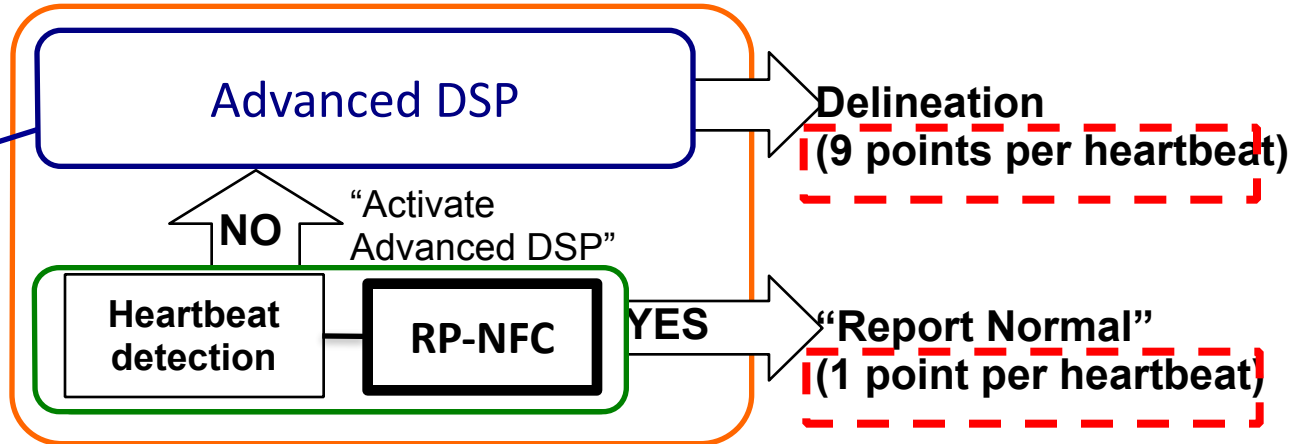
Typical ECG Monitor

Duty Cycle

- Advanced DSP
- Extension
- Idle Time



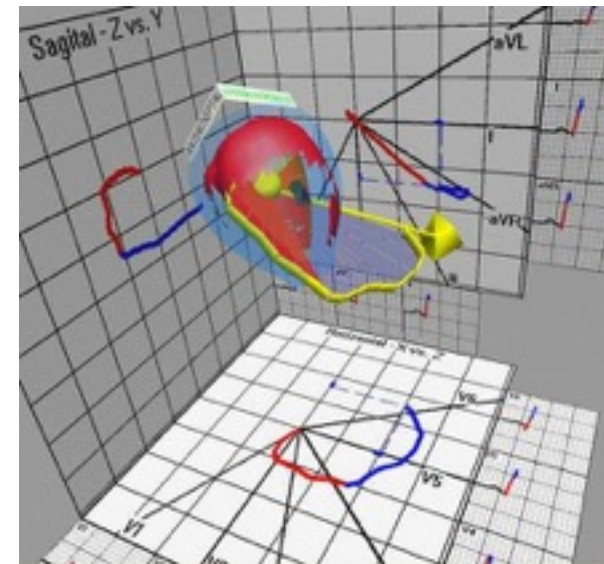
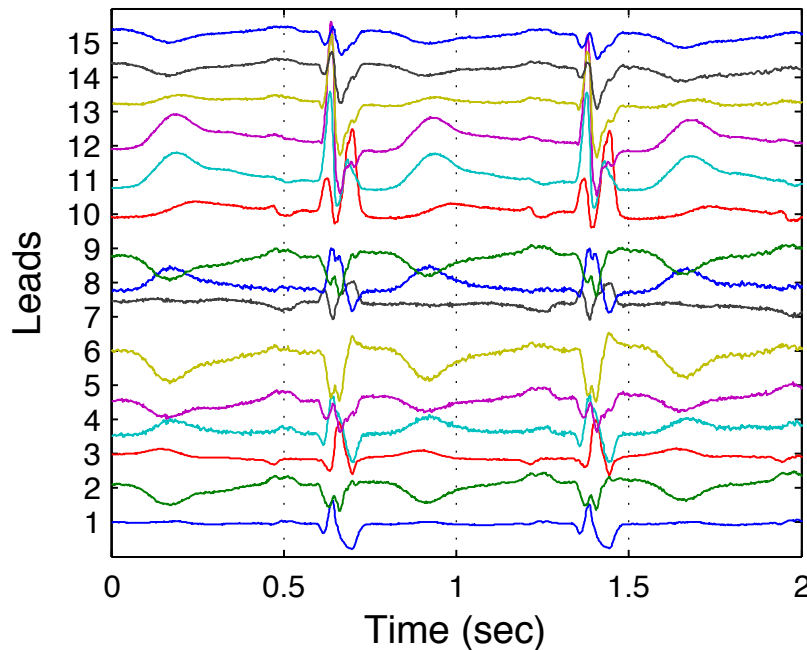
Smarter ECG Monitor



- Duty cycle reduction of 65% for MIT-BIH DB
- Transmission or storage reduction of 68%
- In a real test with multi-core WBSN node
→ Energy savings of 23%

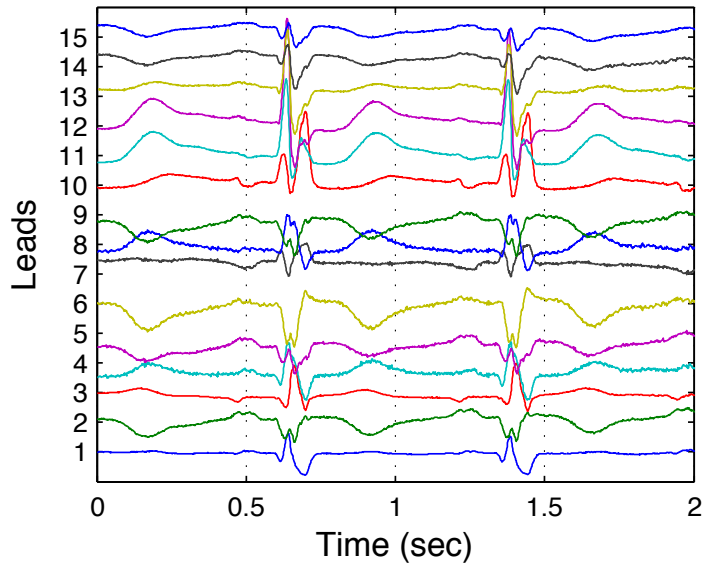
**Up to 61.5 days of operation
(~1476 hours), finally we got
our ULP WBSN!**

- Doctors need multi-lead ECG signals
- ECG leads are different projections of a single multi-dimensional source.

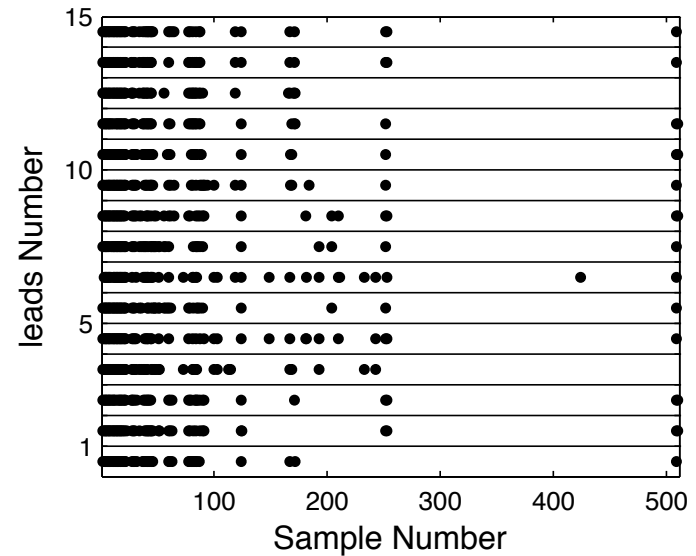


Joint Sparsity Structure

Multi-lead ECG



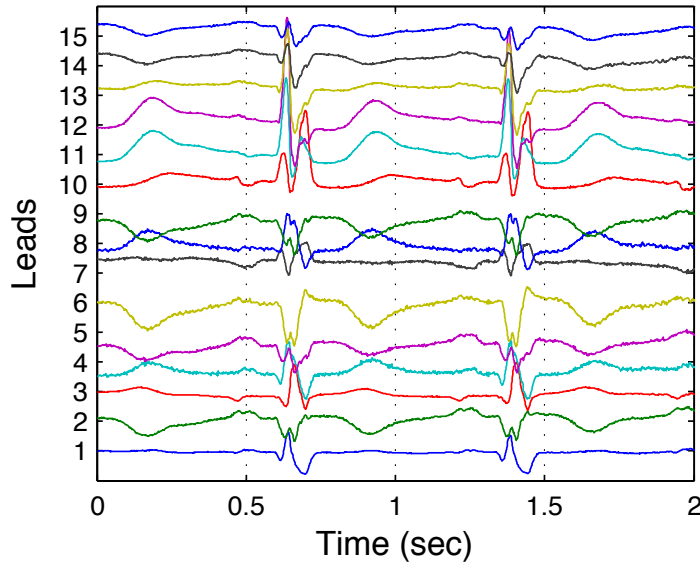
sparse wavelet coefficients



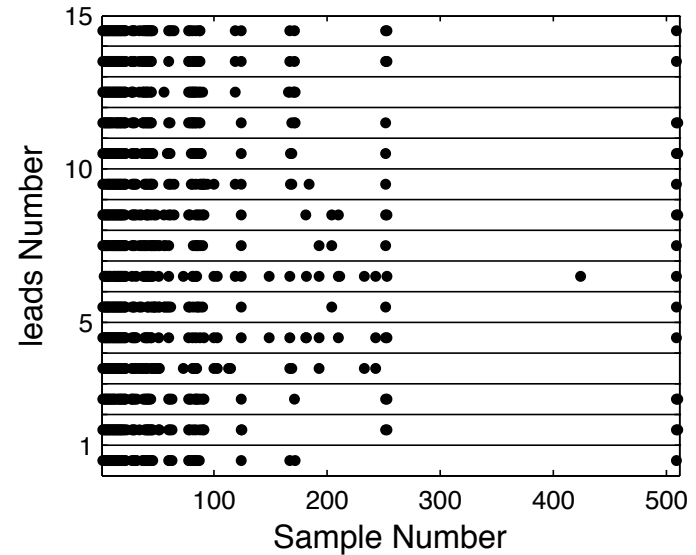
- Strong similarity exist between support of sparse representation among leads.

Joint Sparsity Structure

Multi-lead ECG



sparse wavelet coefficients

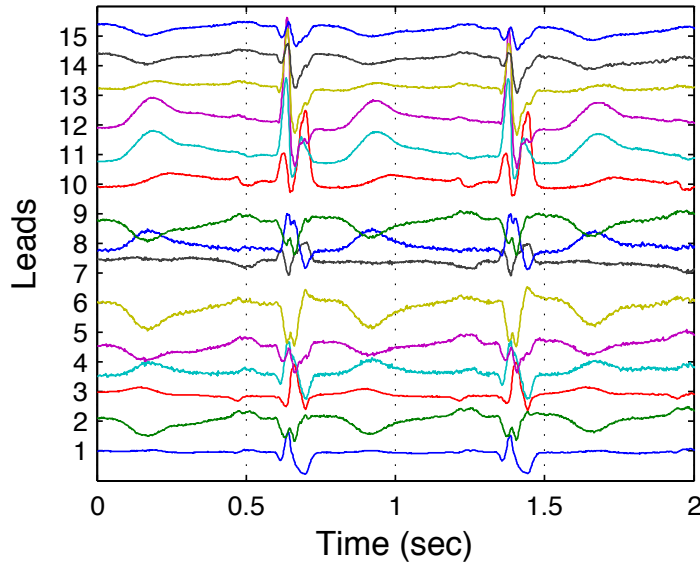


- Strong similarity exist between support of sparse representation among leads.
- Required measurements in normal CS $m = \mathcal{O}(s \log \frac{n}{s})$

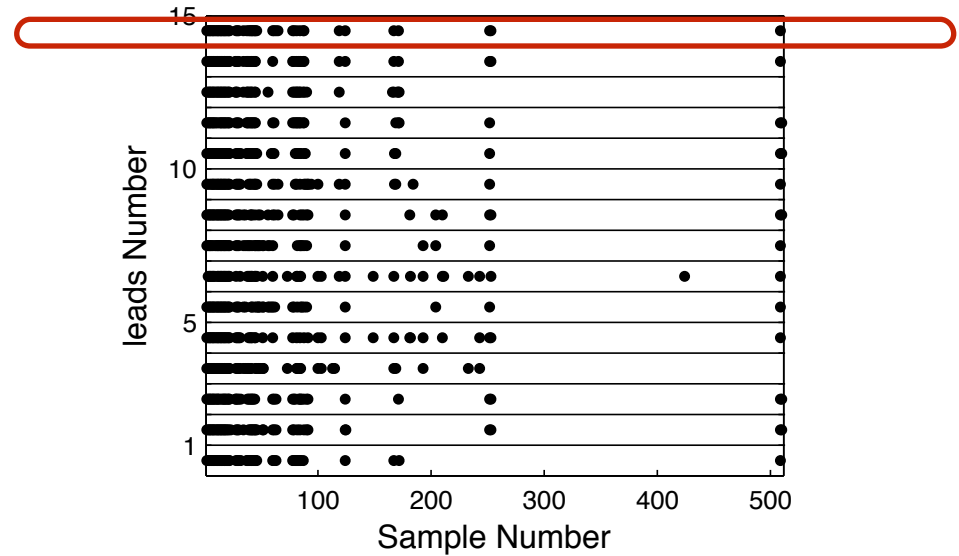
To embed the location
of non-zeros

Joint Sparsity Structure

Multi-lead ECG



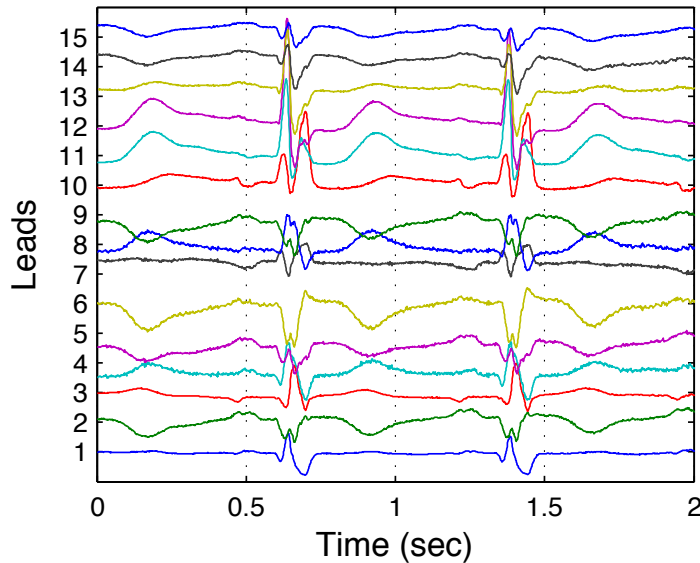
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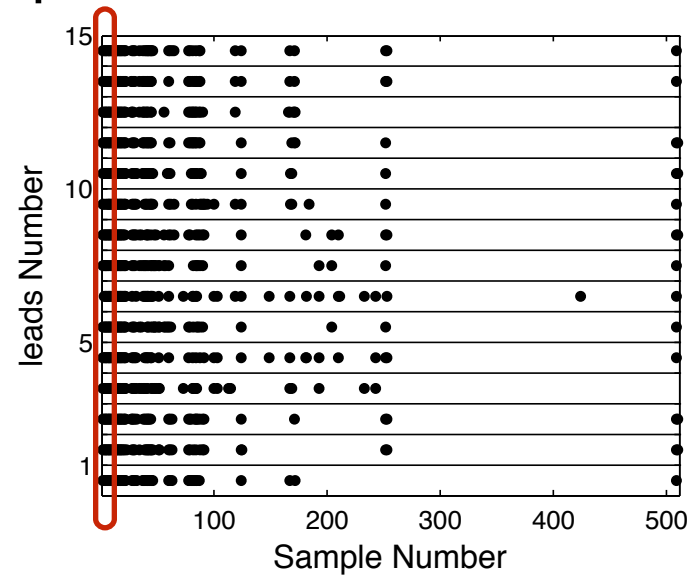
CS:
$$\min_{\hat{\alpha} \in \mathbb{R}^N} \|\hat{\mathbf{A}}\|_1$$
 subject to:
$$\|\Phi\Psi\hat{\mathbf{A}} - \mathbf{y}\|_2 \leq \sigma$$

Joint Sparsity Structure

Multi-lead ECG



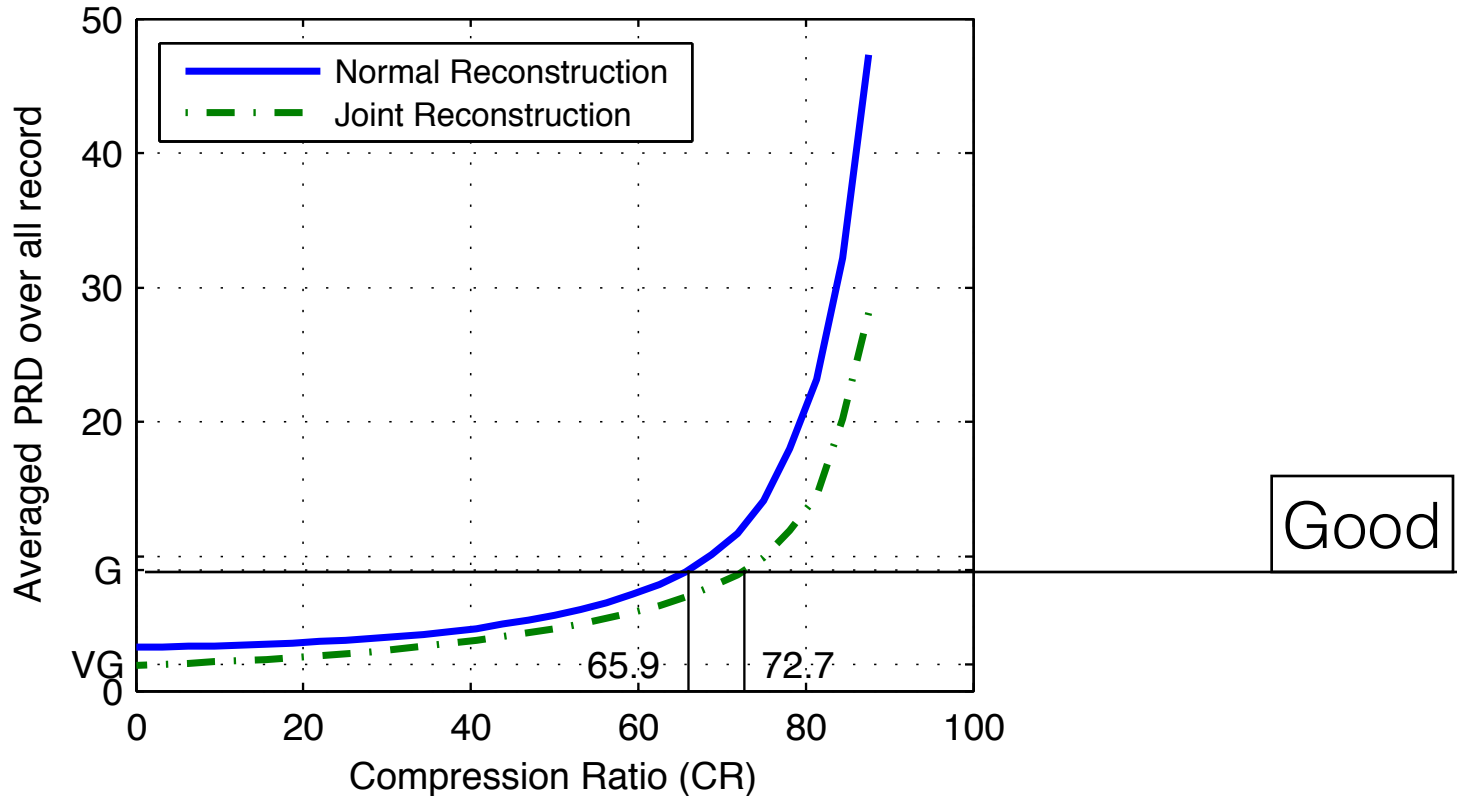
sparse wavelet coefficients



CS:
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Joint comp:
$$\min_{\hat{\alpha} \in \mathbb{R}^N} \|\hat{\mathbf{A}}\|_{1,2} \quad \text{subject to:} \quad \left\| \Phi \Psi \hat{\mathbf{A}} - \mathbf{y} \right\|_2 \leq \sigma$$

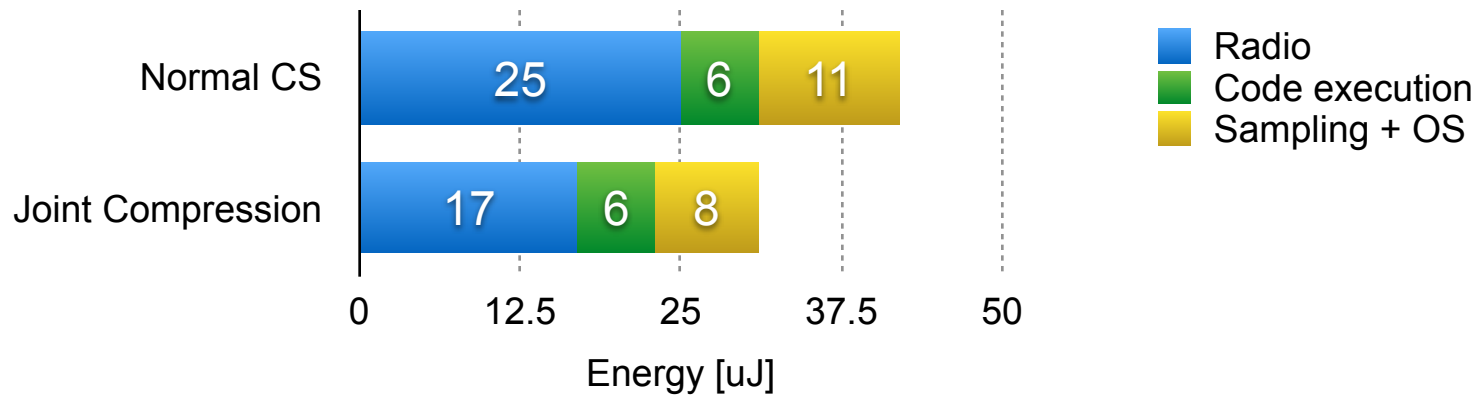
Joint Reconstruction -group sparsity



- **7%** improvement of Compression ratio

Power Consumption breakdown

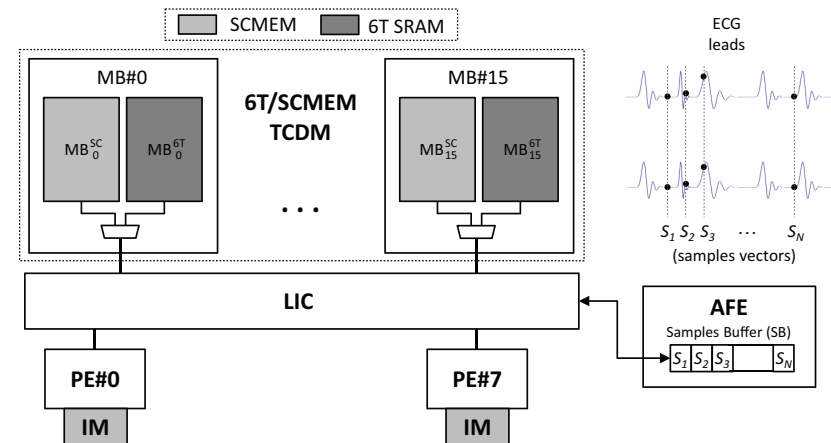
- Power consumption comparison



- 26%** node lifetime extension on top of normal CS (Shimmer Platform)

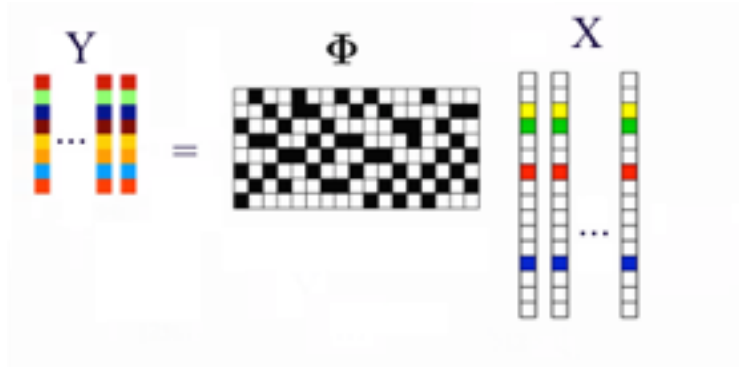
Hybrid Memory on a Multi-core Processor

- Use of reliable Standard Cell (SC) Memories (SCMEM) allows scaling to lower supply voltage, but in cost of large area penalties.
- Use of 6 Transistor SRAM (6T) cell memories are not reliable in supply voltage scaling.
- Ultra-low power multi-core architecture for multi-channel bio-signal processing.
- Hybrid memory architecture with 6T SRAM and SCMEM working on a aggressive voltage scaling.



Architecture designed by
university of Bologna

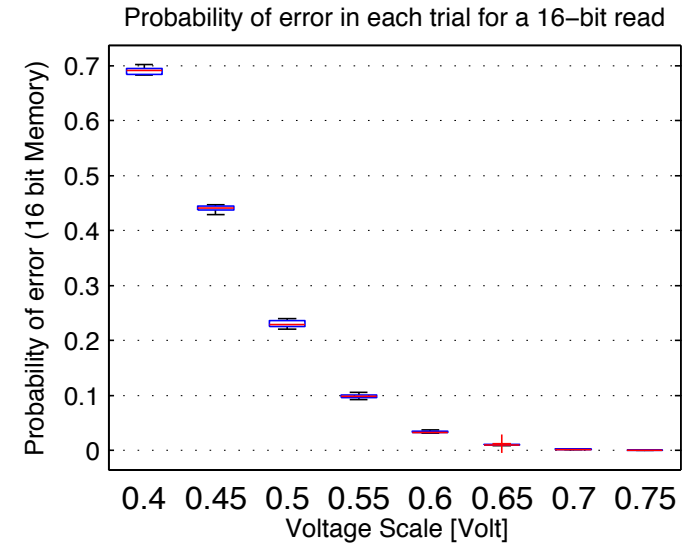
- Sensing Matrix is stored in 6TMEMs



- Sensing Matrix is stored in 6TMEMs
- Joint comp:

$$Y = \Phi X = \Phi \Psi A$$

$$\min_{\hat{\alpha} \in \mathbb{R}^N} \|\hat{A}\|_{1,2} \quad \text{subject to:} \quad \|\Phi \Psi \hat{A} - Y\|_2 \leq \sigma$$



- Sensing Matrix is stored in 6TMEMs
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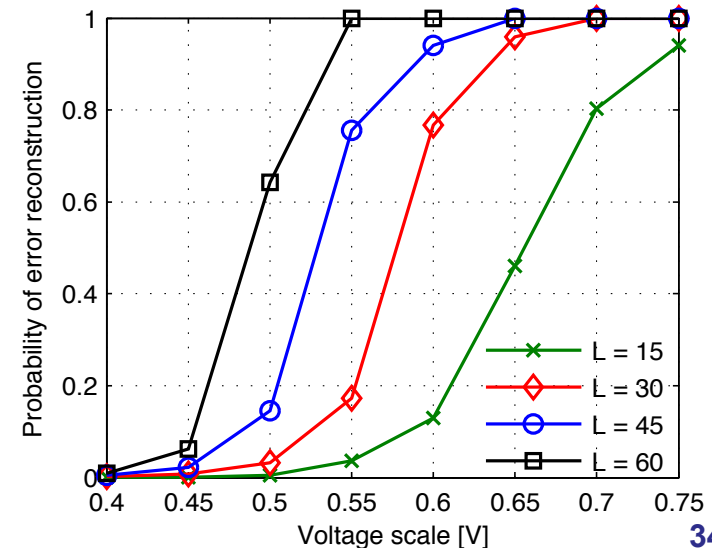
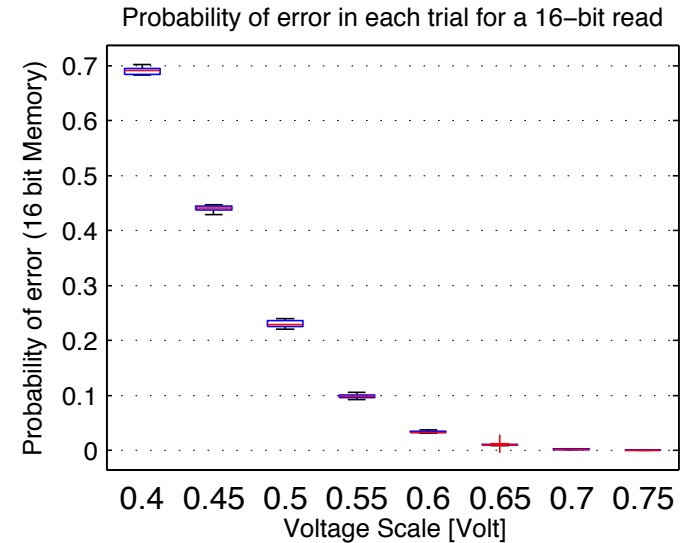
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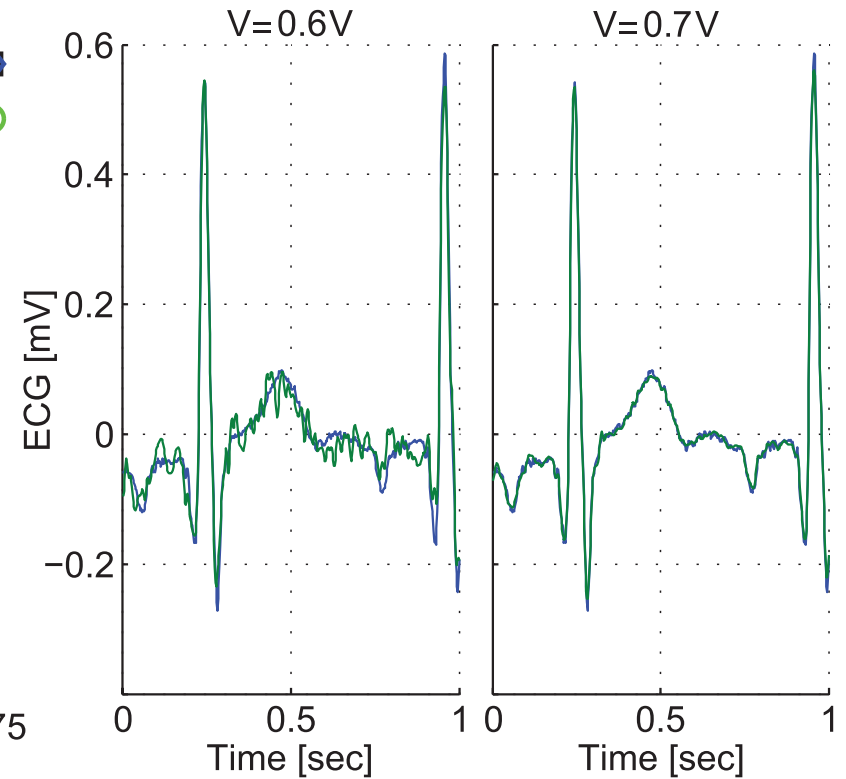
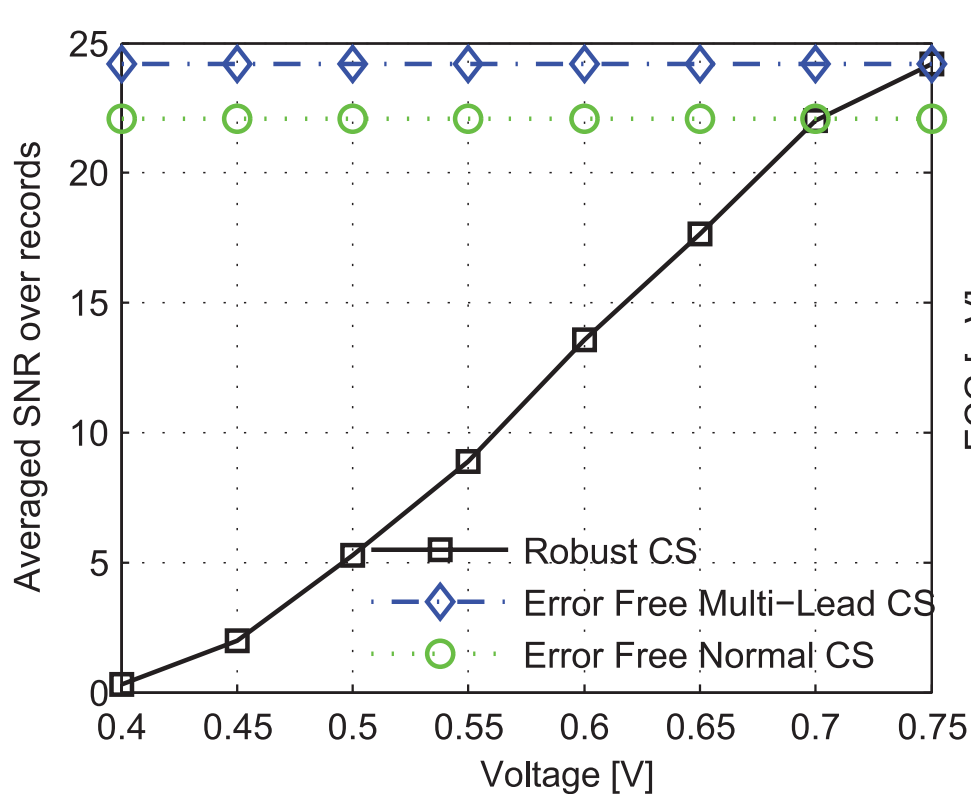
- Joint comp with Error:

$$Y = (\Phi + E)X = (\Phi + E)\Psi A$$

- **Robust Compressed Sensing**

$$\min_{\hat{A}, \hat{E}} \|\hat{A}\|_{1,2} + \lambda \|\hat{E}\|_1 \quad \text{s.t.:} \quad \|(\Phi + \hat{E})\Psi \hat{A} - Y\|_2 \leq \sigma$$

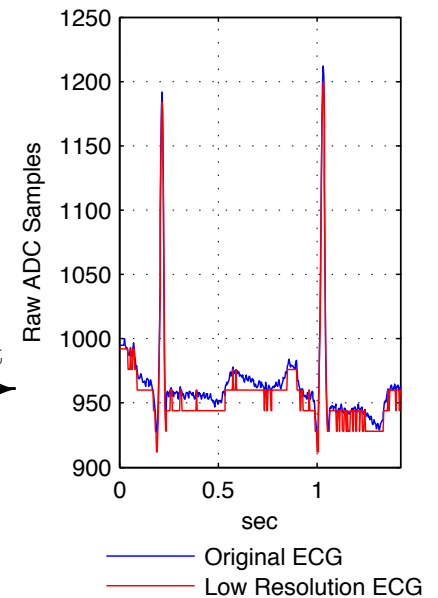
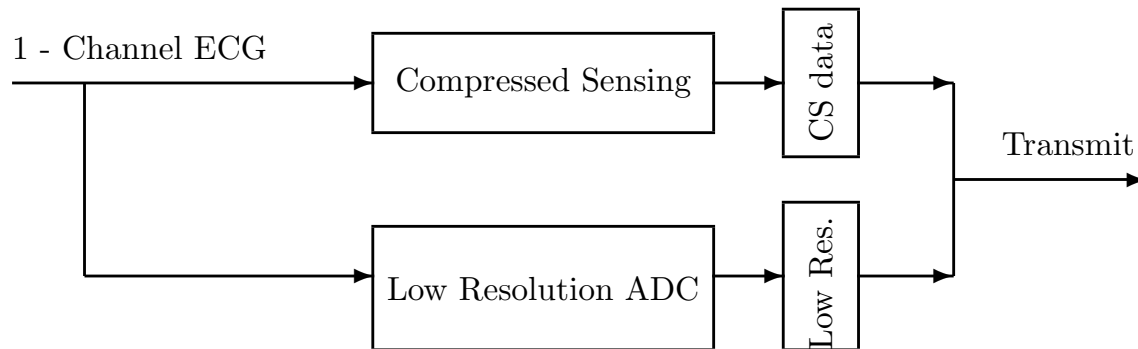




Design reach to **60%** reduction in Power consumption
with a **13%** area overhead

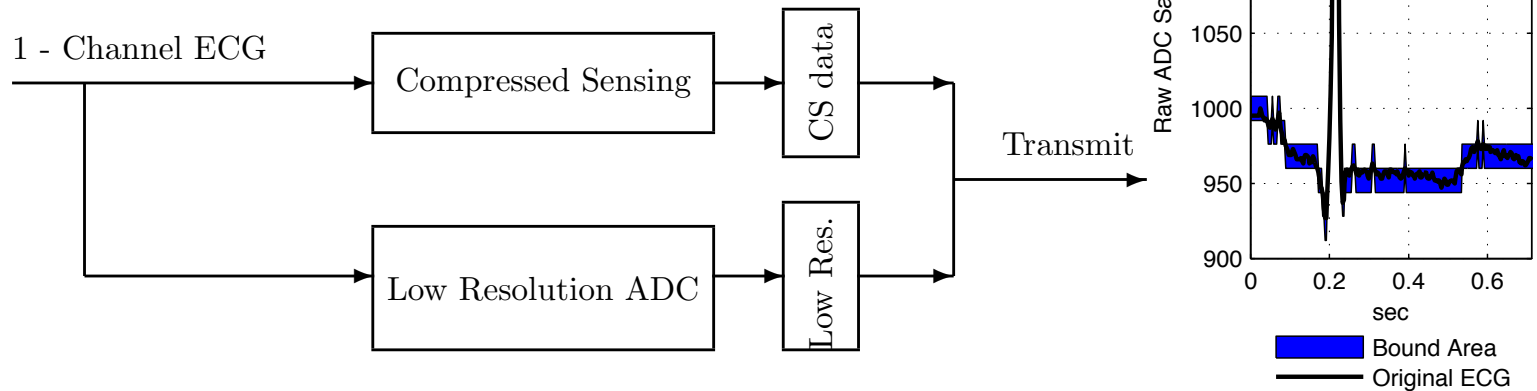
Hybrid CS-based Front-end

- New hybrid digital+analog design is proposed
 - Parallel low resolution channel
 - High resolution RMPI channel



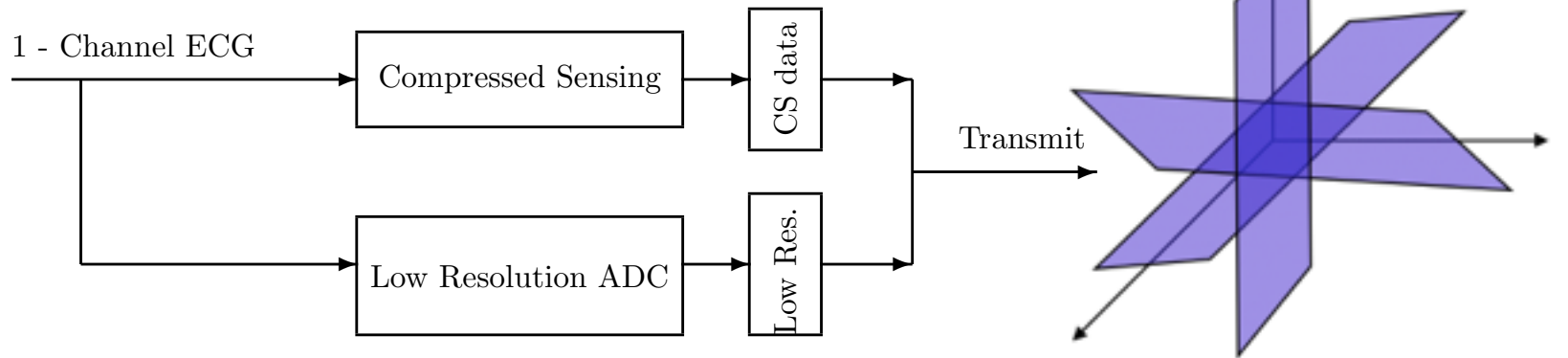
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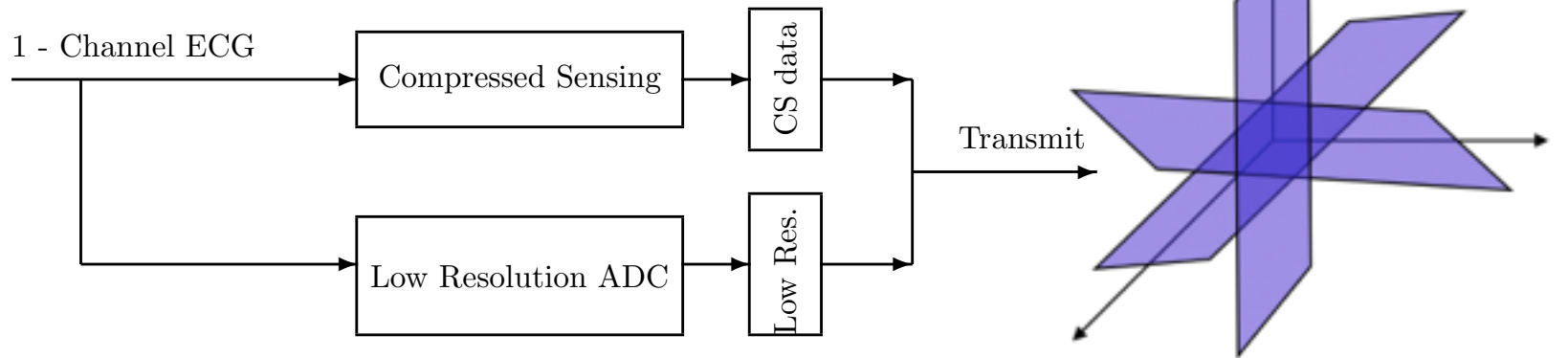
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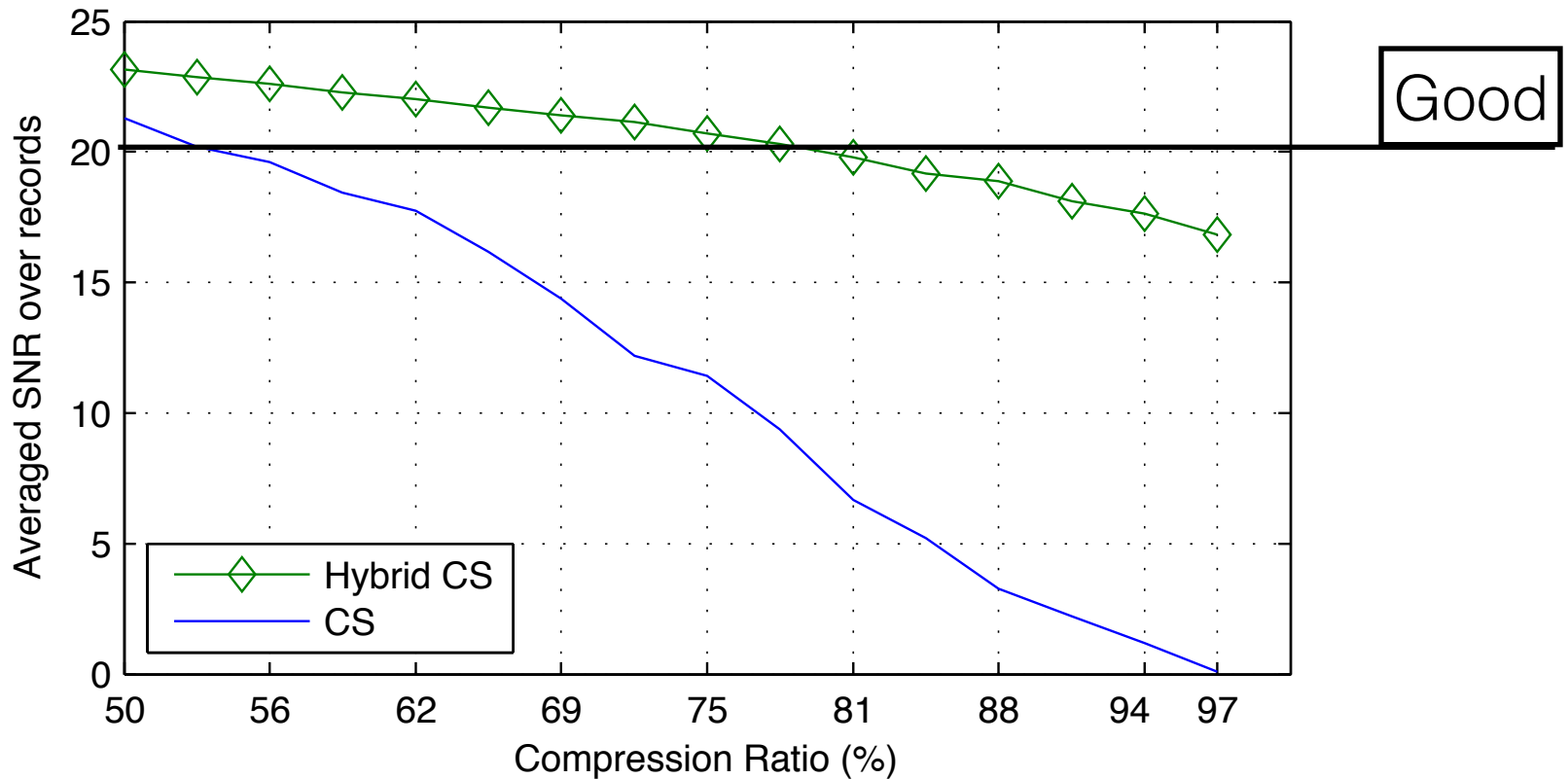
- New hybrid digital+analog design is proposed
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$$\min_{\tilde{\alpha} \in \mathbb{R}^N} \|\tilde{\alpha}\|_1 \quad \text{subject to} \quad \begin{cases} \|\Phi\Psi\tilde{\alpha} - \mathbf{y}\|_2 \leq \sigma, \\ \dot{\mathbf{x}} \leq \Psi\tilde{\alpha} \leq \dot{\mathbf{x}} + d \end{cases}$$

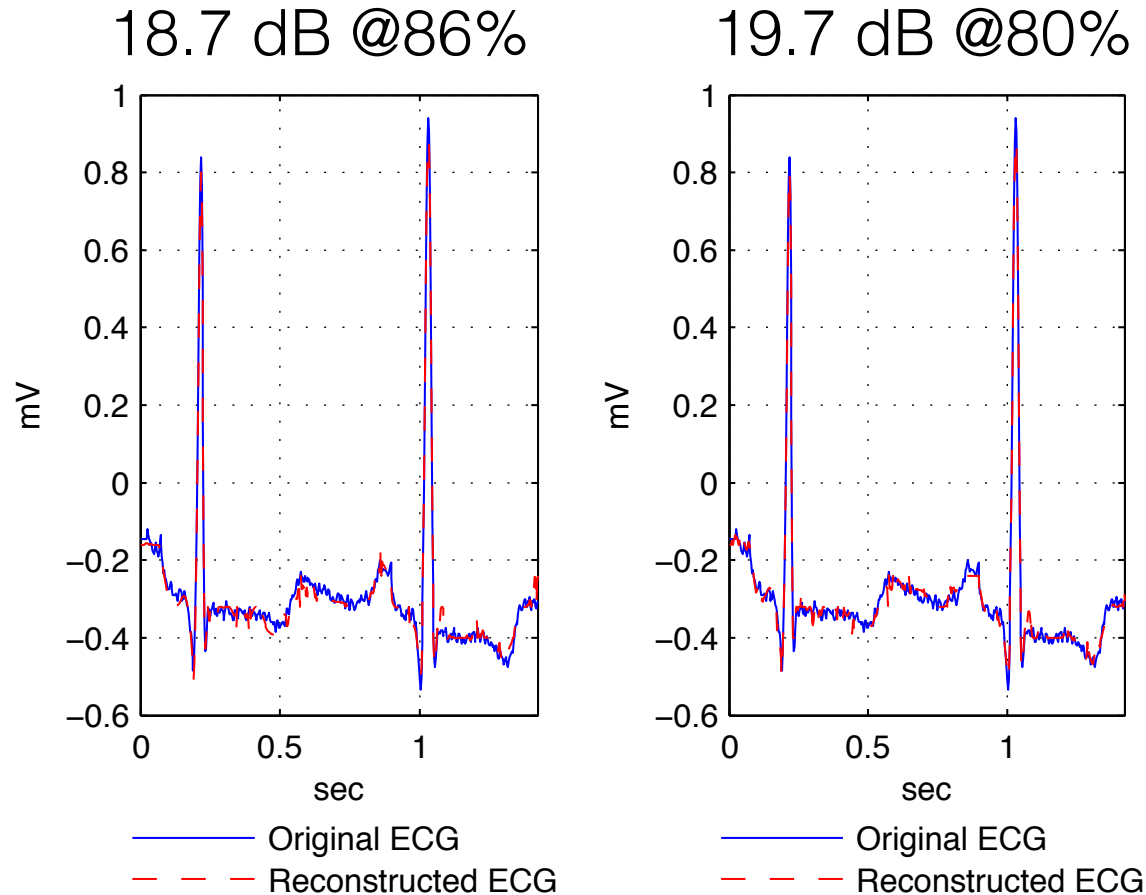
- **Relaxed RIP, fewer measurements**

Performance Quality Comparison



- **35 %** reduction in compression ratio
- Very good performance at higher CR (SNR = 17dB @97%)

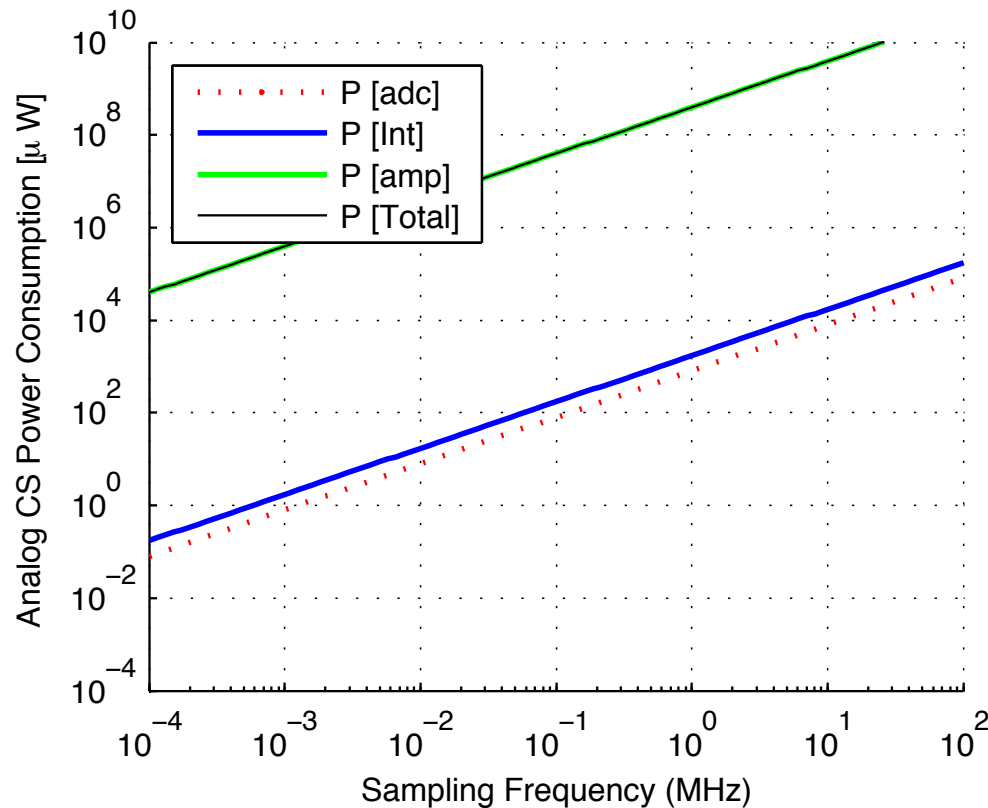
Performance Quality Comparison



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Power consumption break-down

- Power break-down



2.5 X Power reduction compared to RMPI at Good quality
11 X reduction at SNR = 17dB (number of channels = 16)

Conclusion

- Smart ULP WBSN nodes needed to enable new healthcare
 - Feasible to do real-time automated biosignals analysis
 - Communication not always the worst part: sensing and processing
- Knowledge about target bio-signals not to overdesign WBSNs
 - Compressed sensing very powerful approach (if used with care)
 - Removes need for complex instructions sets and limits memory use
- New ULP WBSN multi-parametric architectures coming up
 - Adaptive to each patient (big data link!)
 - Joint compressive sensing can help to significantly save power

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- New ULP WBSN multi-parametric architectures coming up
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 - Joint compressive sensing can help to significantly save power
- Novel field: wearable multimodal biosignal systems
 - **Develop uses of these new WBSNs to monitor other emotions, etc.**
 - **Design methods to ease low-power software mapping needed!**

Thank You



QUESTIONS?

Acknowledgments:



PHIDIAS and ICT energy



ObeSense, BodyPowerSense,
BioCS Projects in Nano-Tera.ch

Thanks to our great collaborators:
LTS2-EPFL, TCL-EPFL and IIS-ETHZ

Key References and Bibliography

- **CS-based ECG Compression and implementation**
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